

# ARTIFICIAL MECHANICAL SYSTEMS for the UPPER EXTREMITY

DICK H. PLETTENBURG

BIOMECHATRONICS WB2432

**2007-03-07 STATE OF THE ART IN UE PROSTHETICS**

**2007-03-14 CONTROL**

**2007-03-21 ACTUATION**

# ACTUATION OF UPPER EXTREMITY PROSTHETICS

# PROSTHESES

CONTROL

ALWAYS BY THE BODY

MECHANICAL

ELECTRICAL

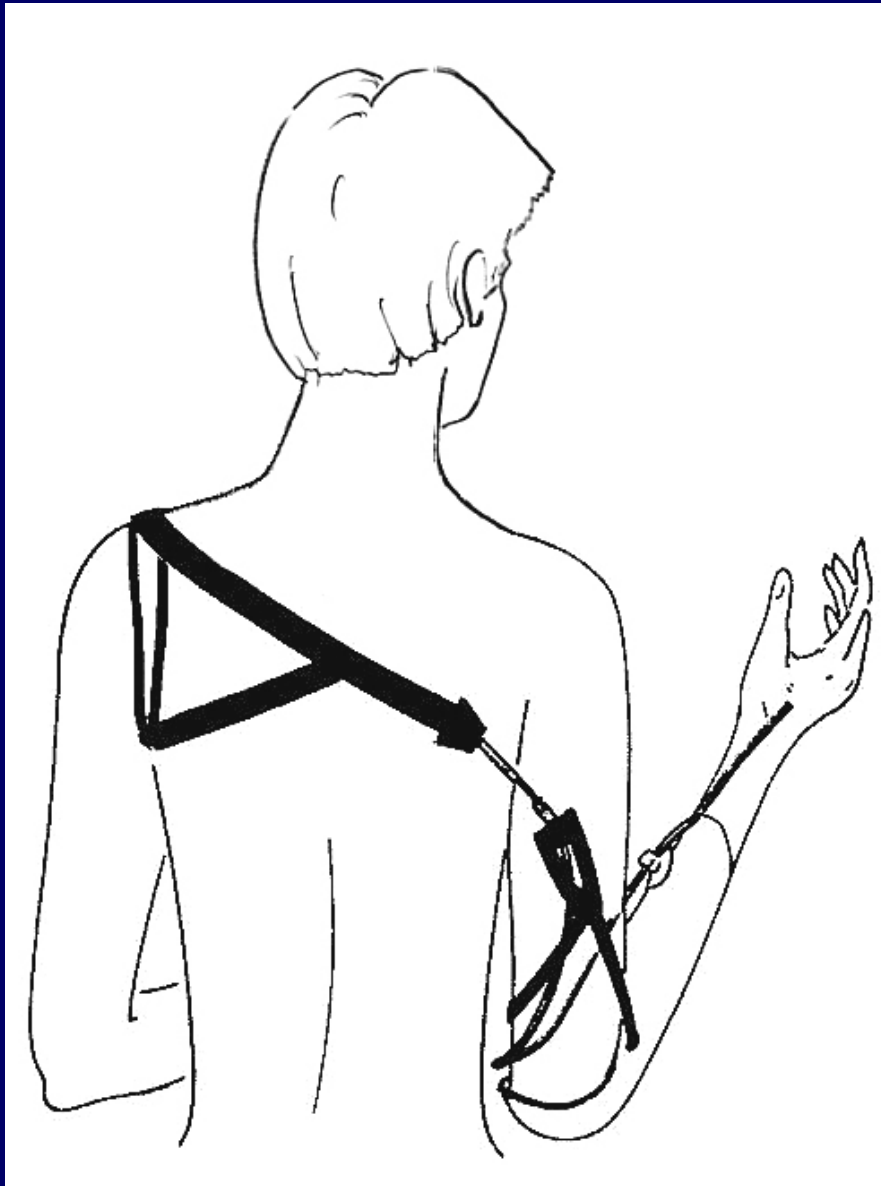
POWER

FROM THE BODY

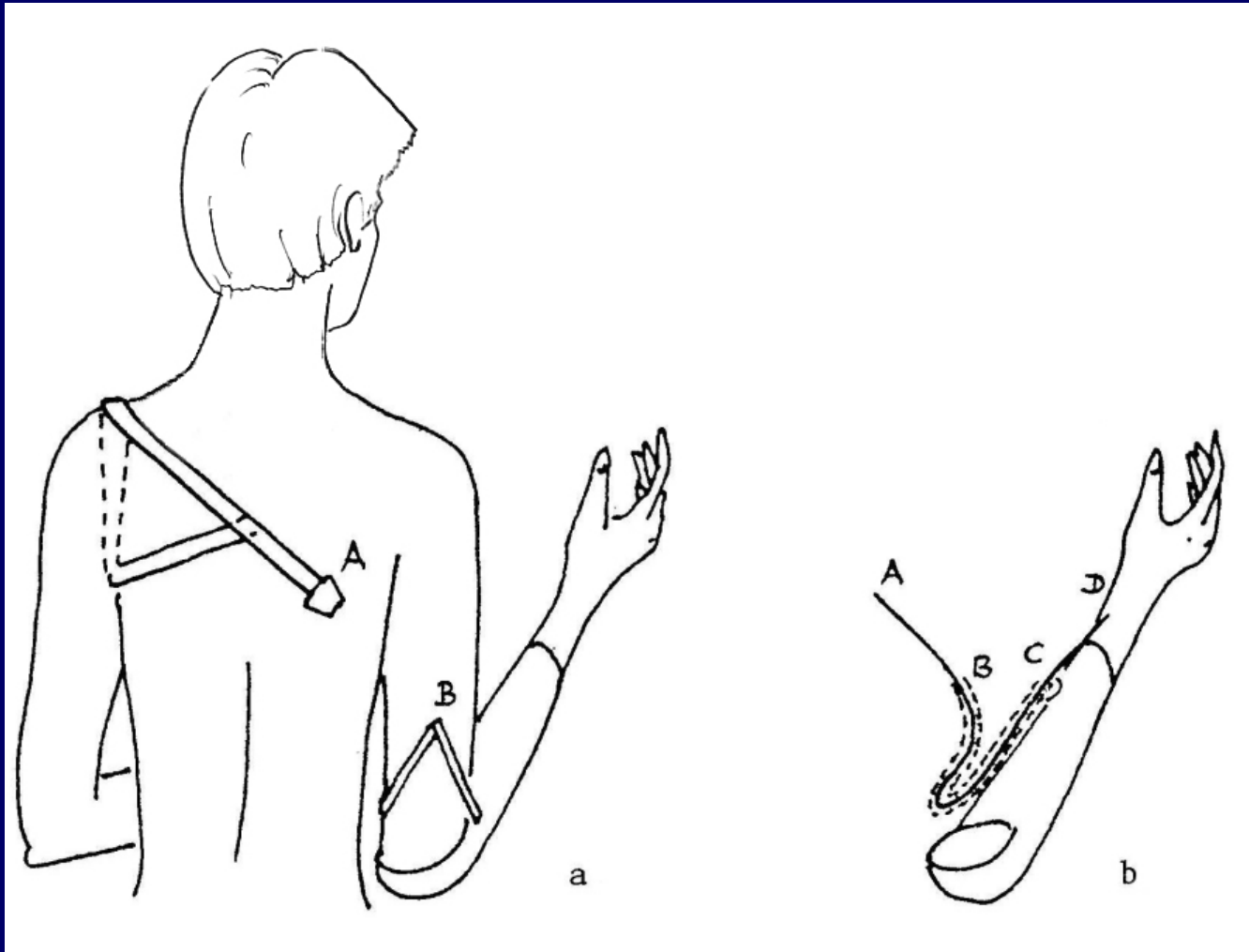
EXTERNALLY

# BODY POWER

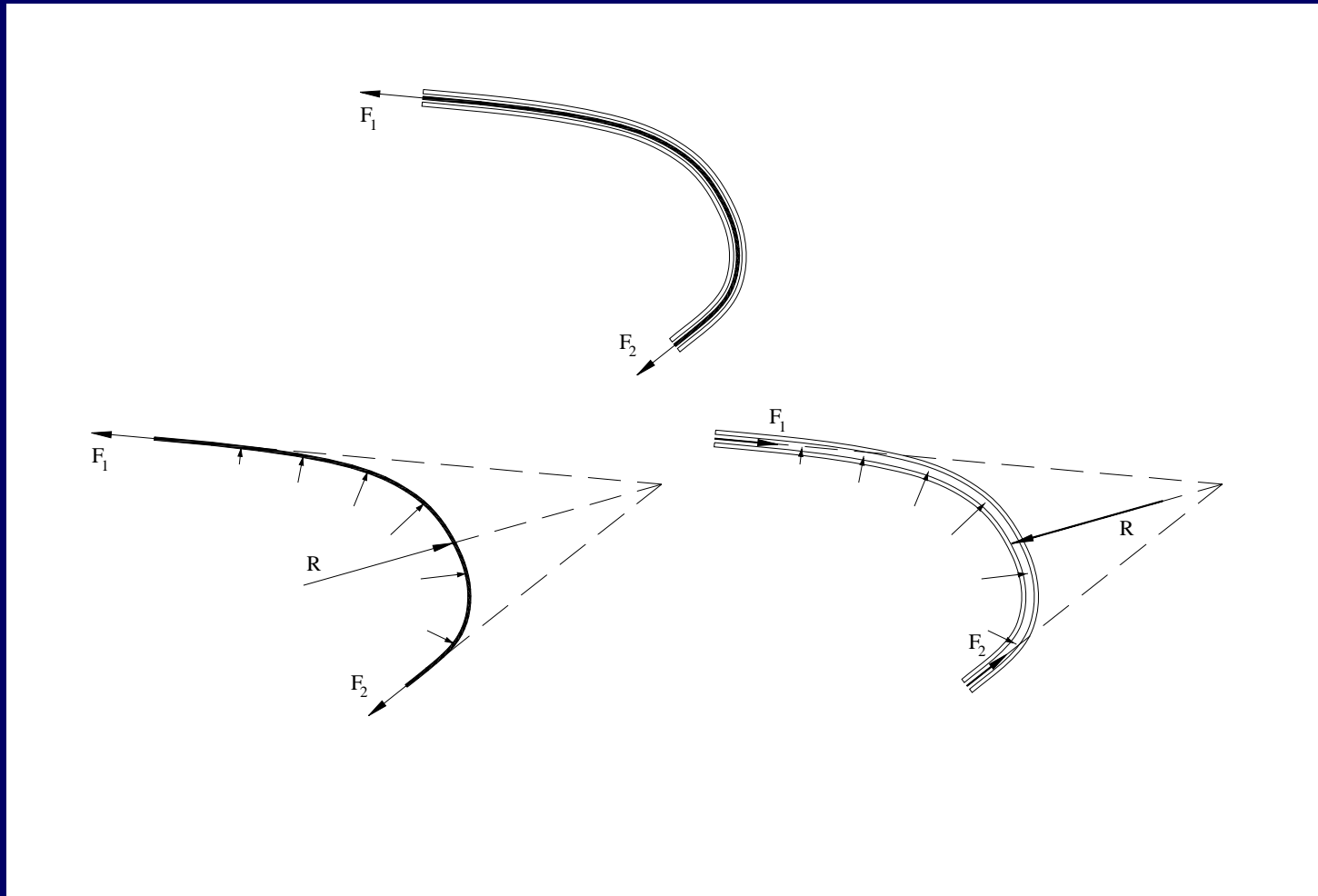
# STRAPS



# STRAPS

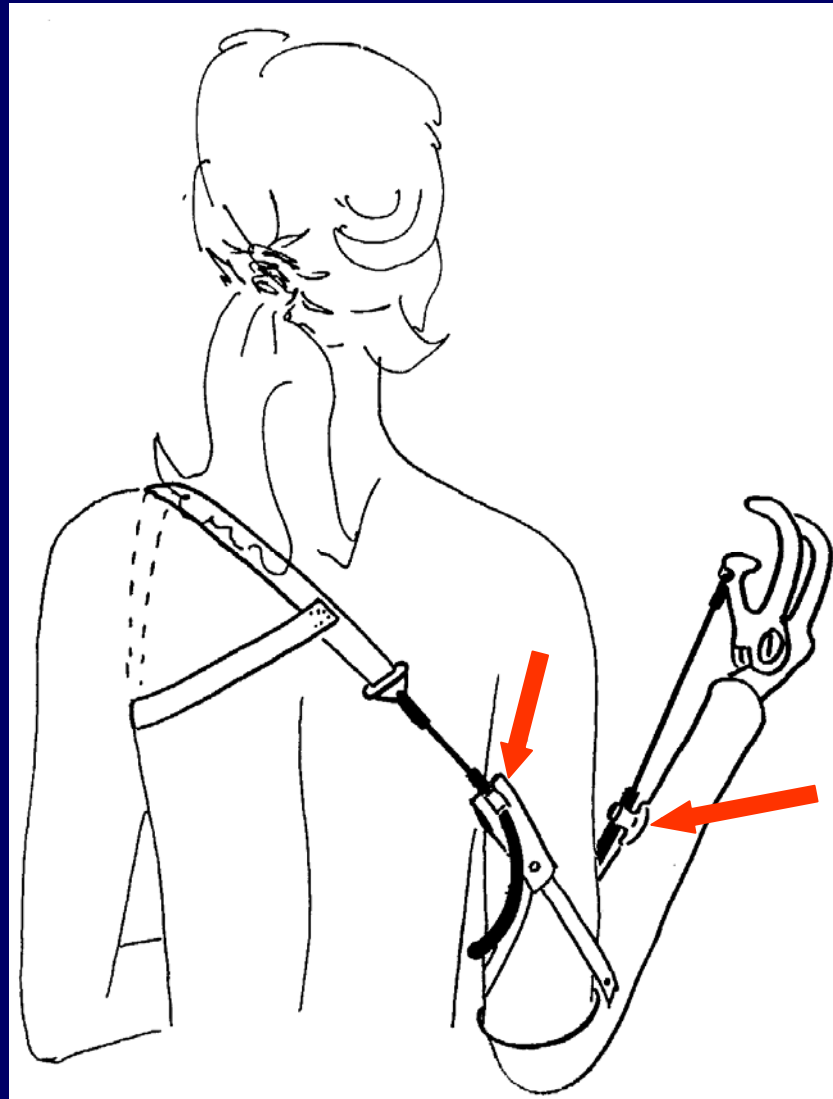


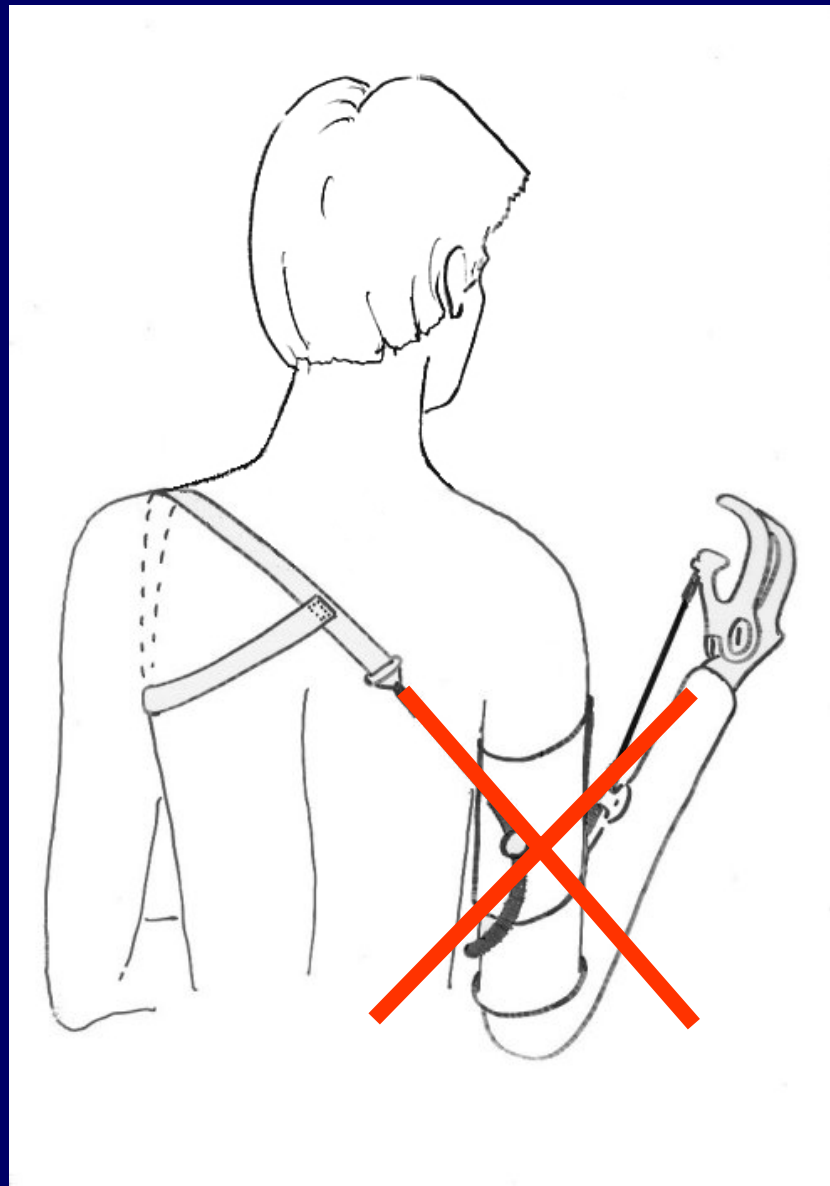
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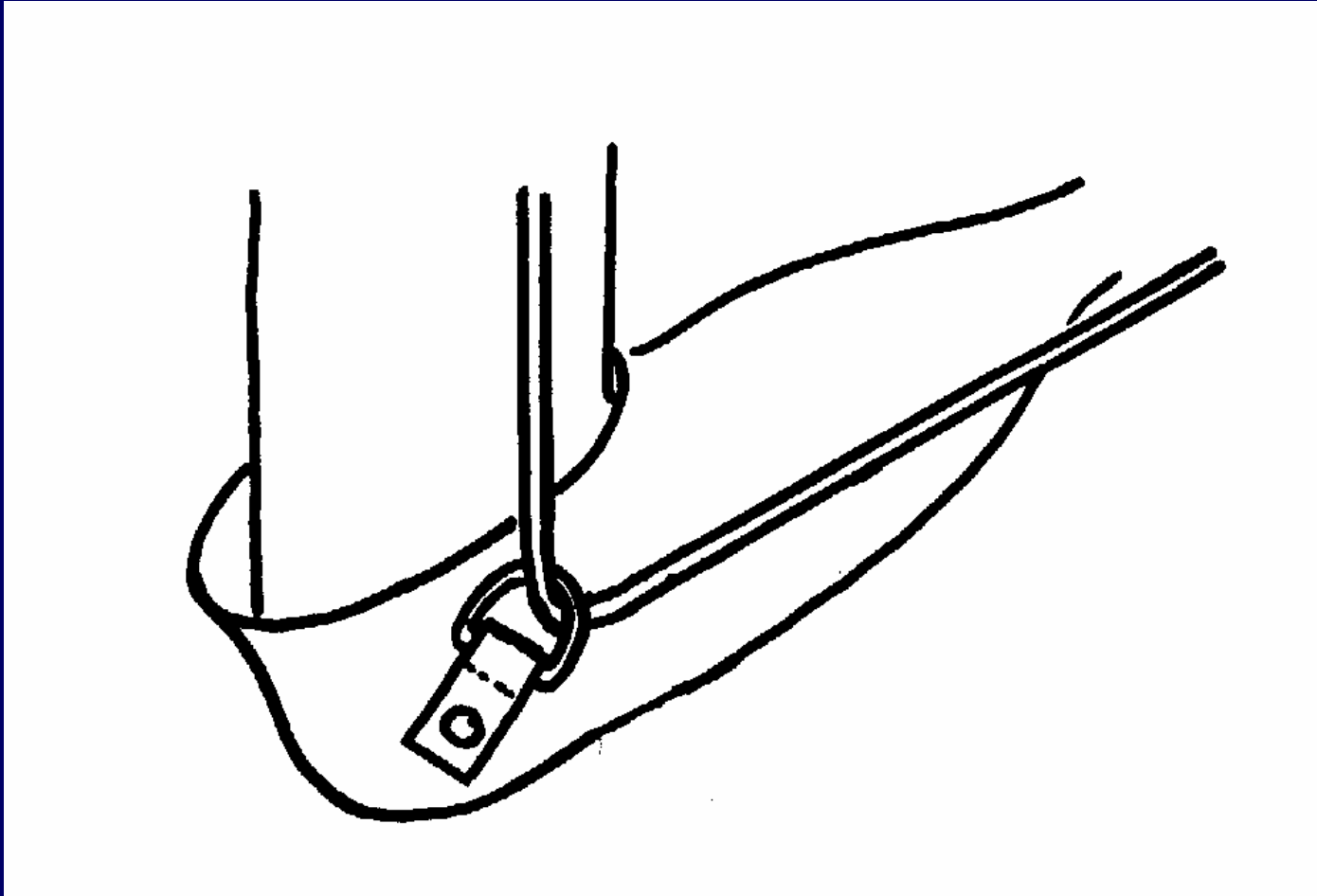


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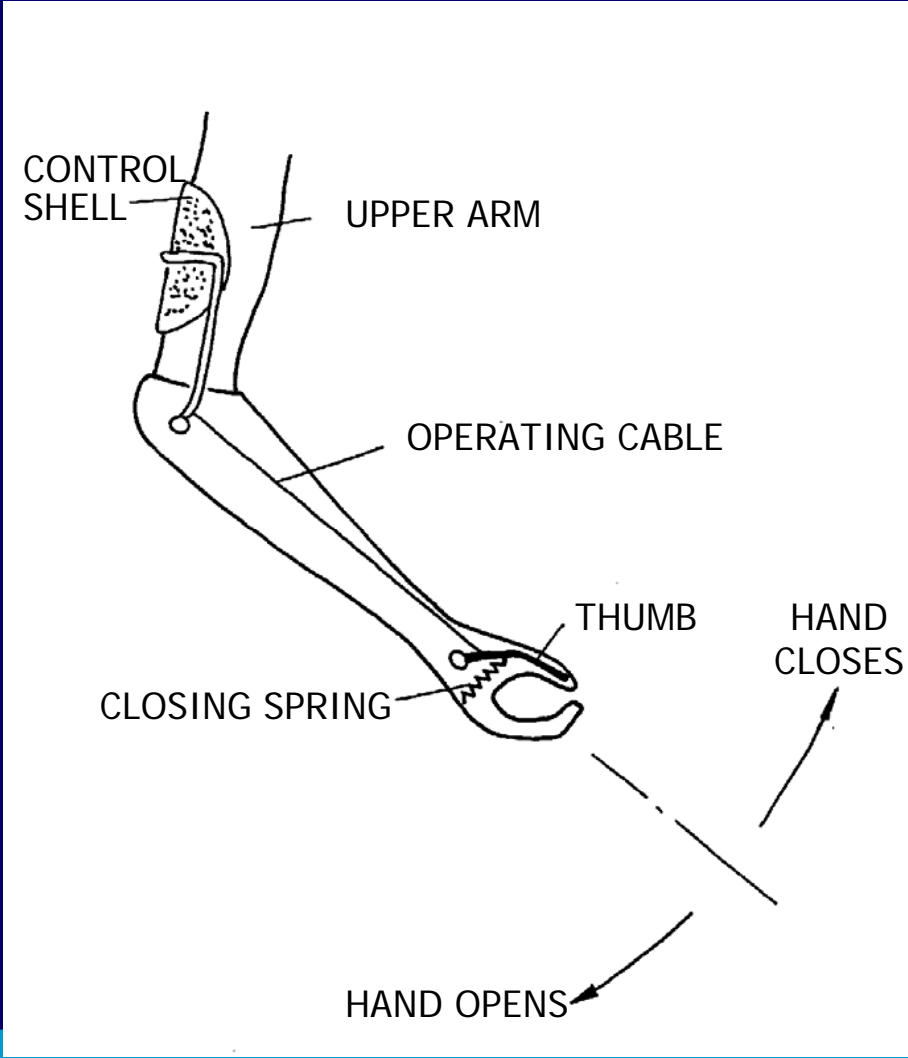




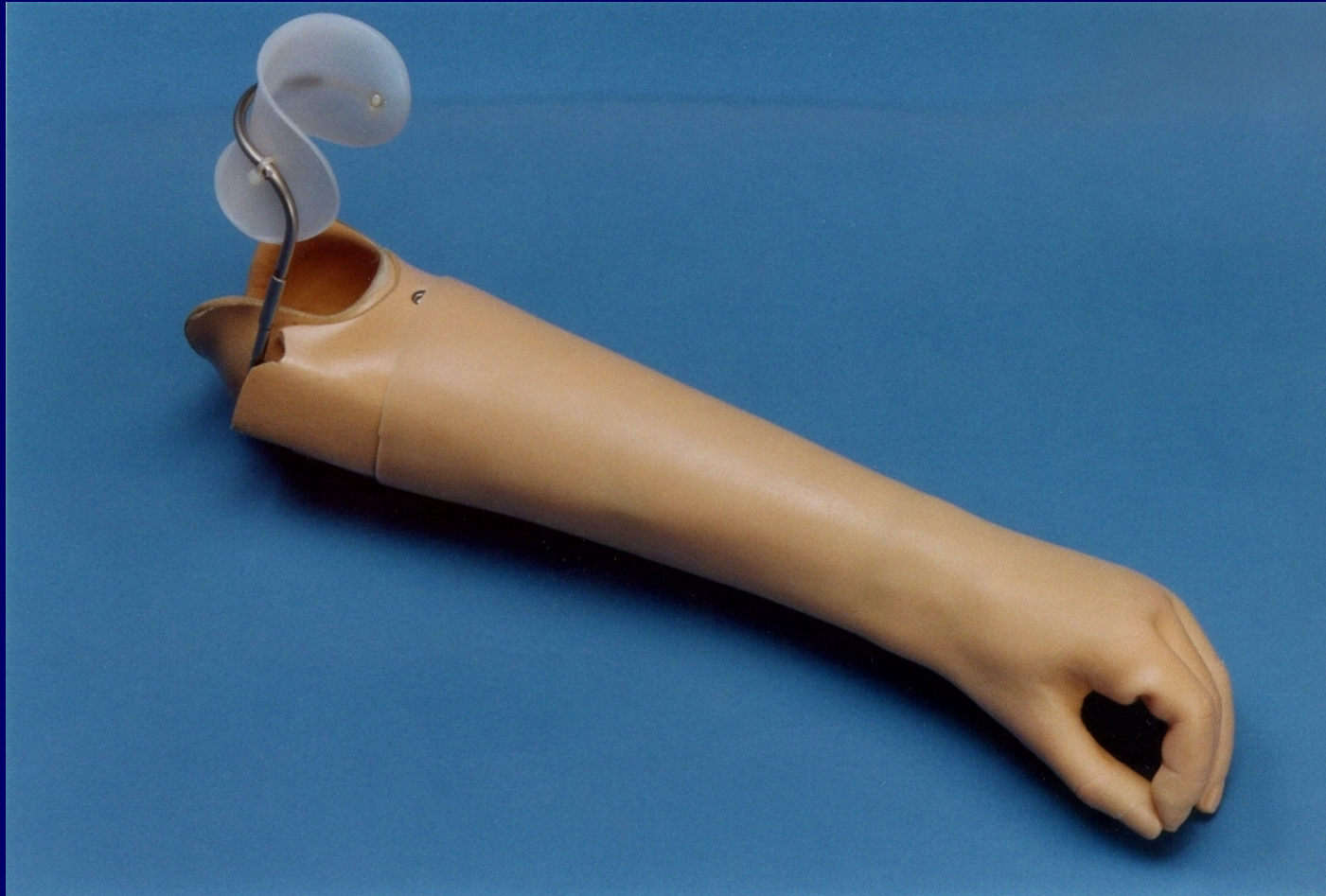
# STRAPS



# ELBOW CONTROL



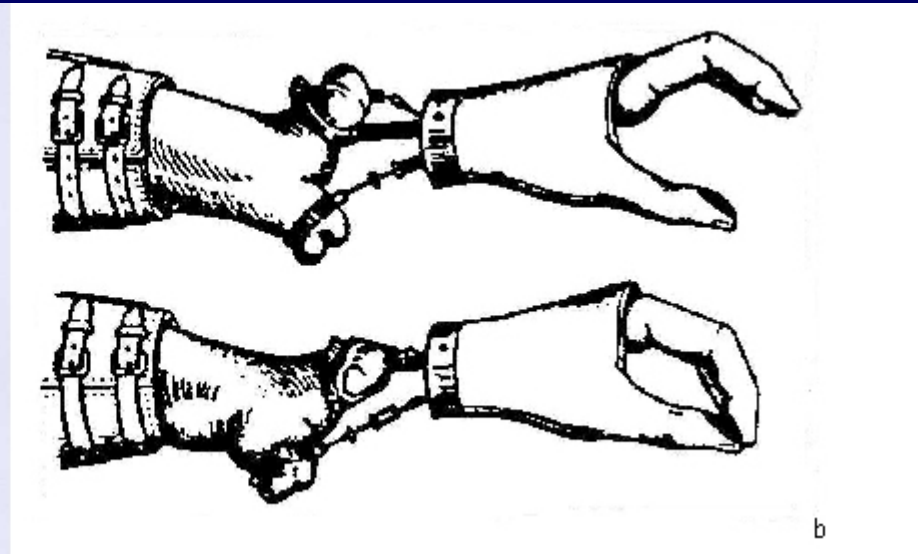
# ELBOW CONTROL



# CINEPLASTY: GIULIANO VANGHETTI 1898



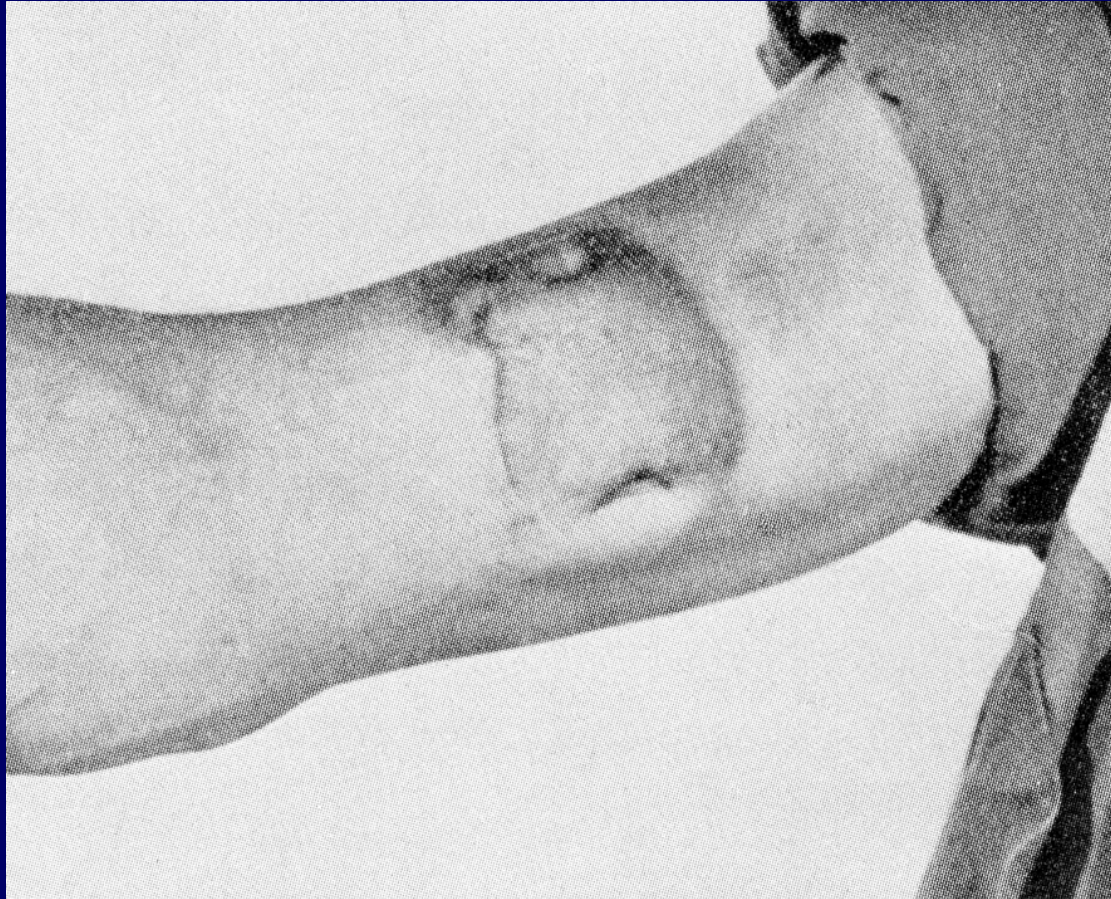
# CINEPLASTY: GIULIANO VANGHETTI



Weir, 1998



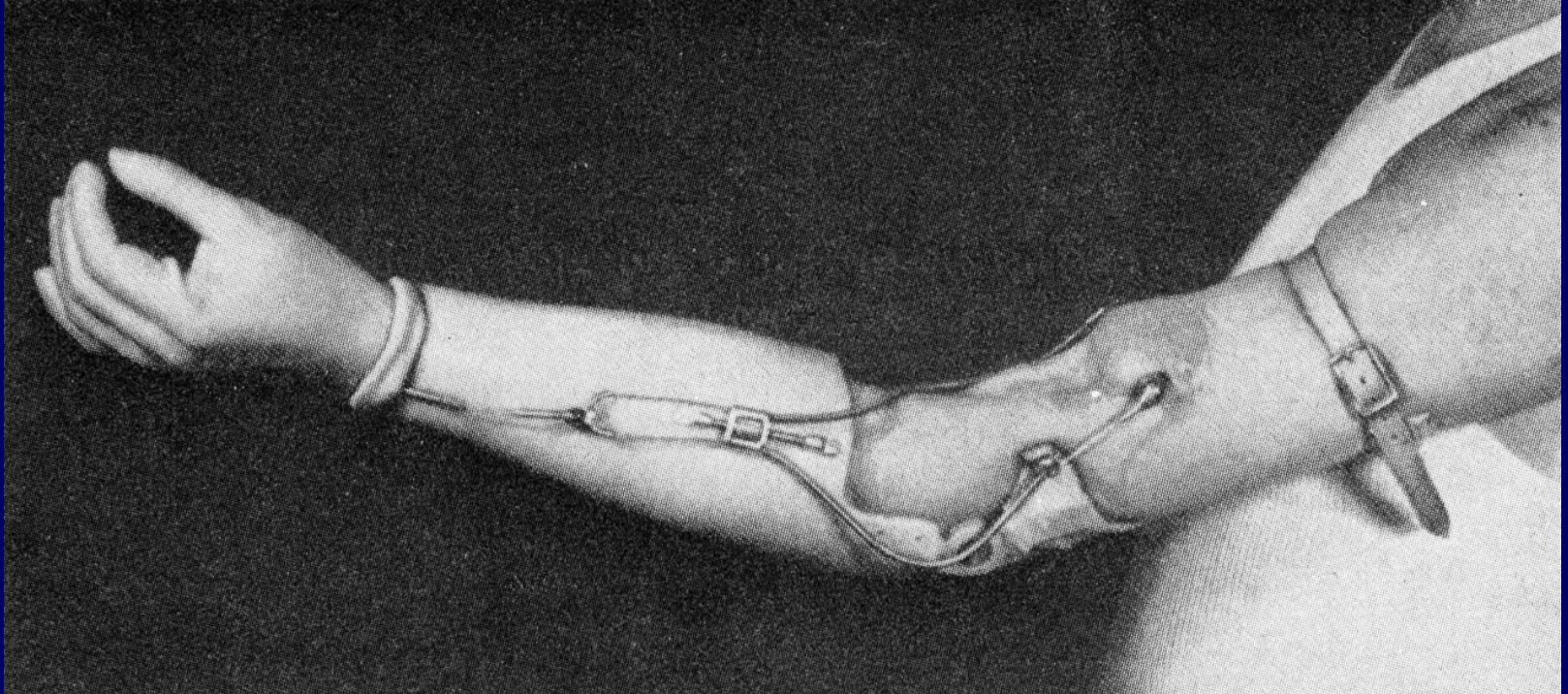
# CINEPLASTY: FERDINAND SAUERBRUCH 1915



Klopsteg & Wilson, 1954



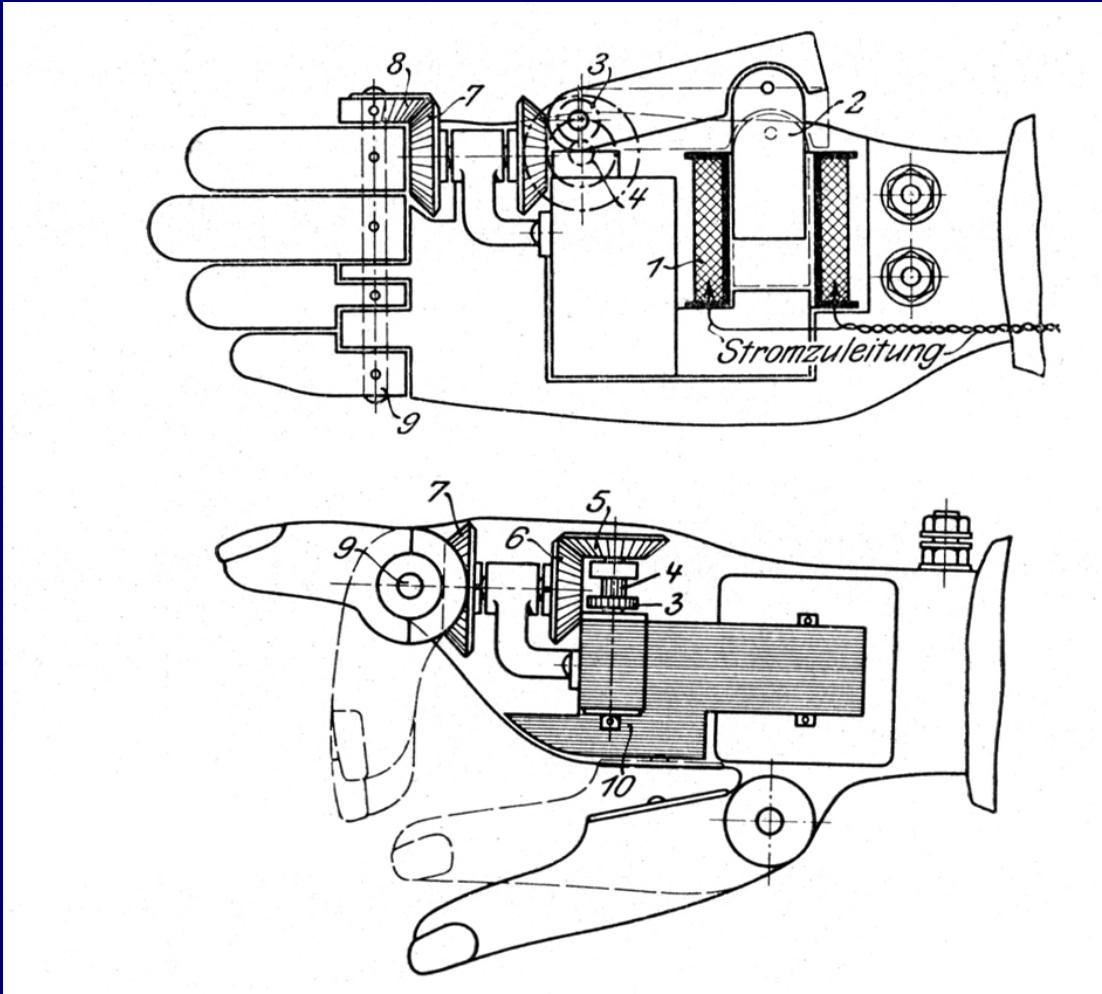
# CINEPLASTY: FERDINAND SAUERBRUCH



Klopsteg & Wilson, 1954

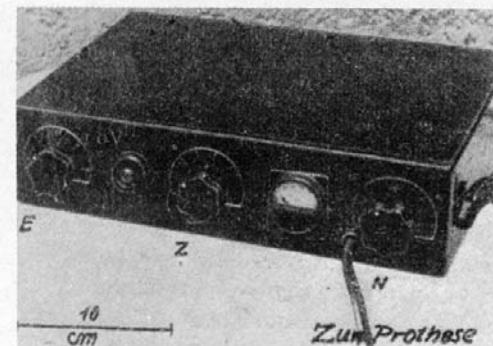
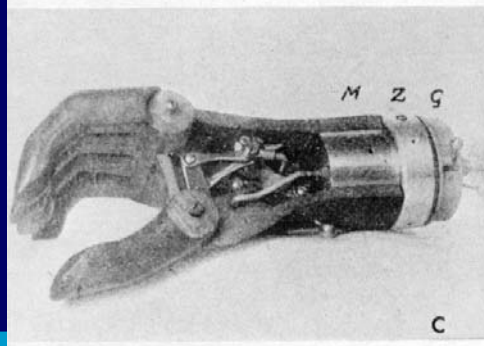
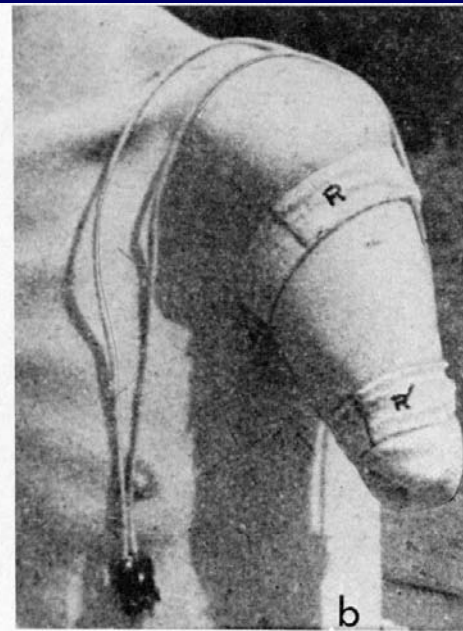
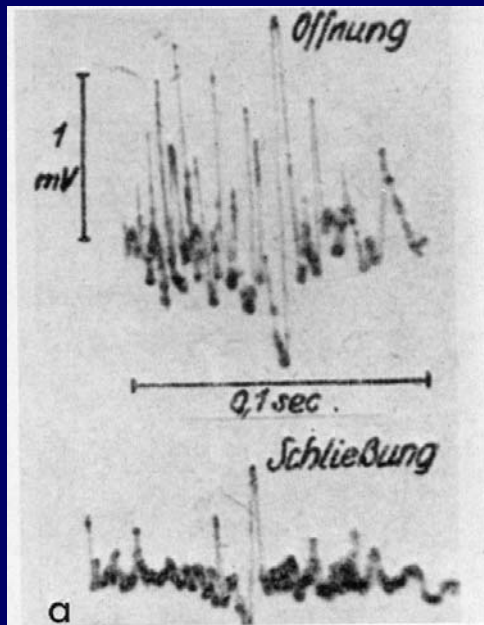
# EXTERNAL POWER

# ELECTRICAL



Borchardt et.al., 1919

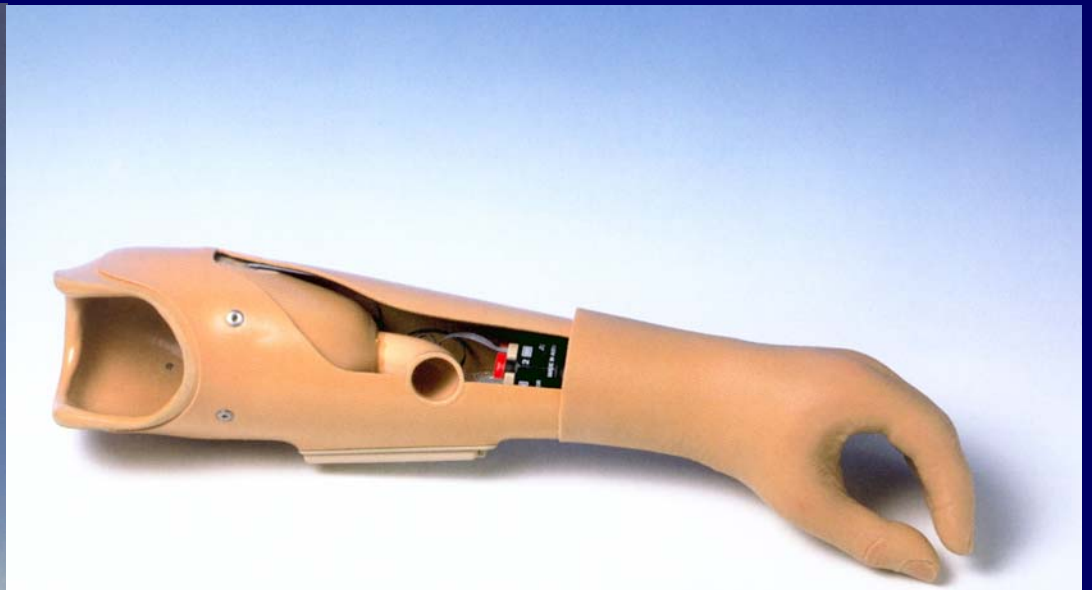
# ELECTRICAL: REITER 1948



Childress & Billock, 1970

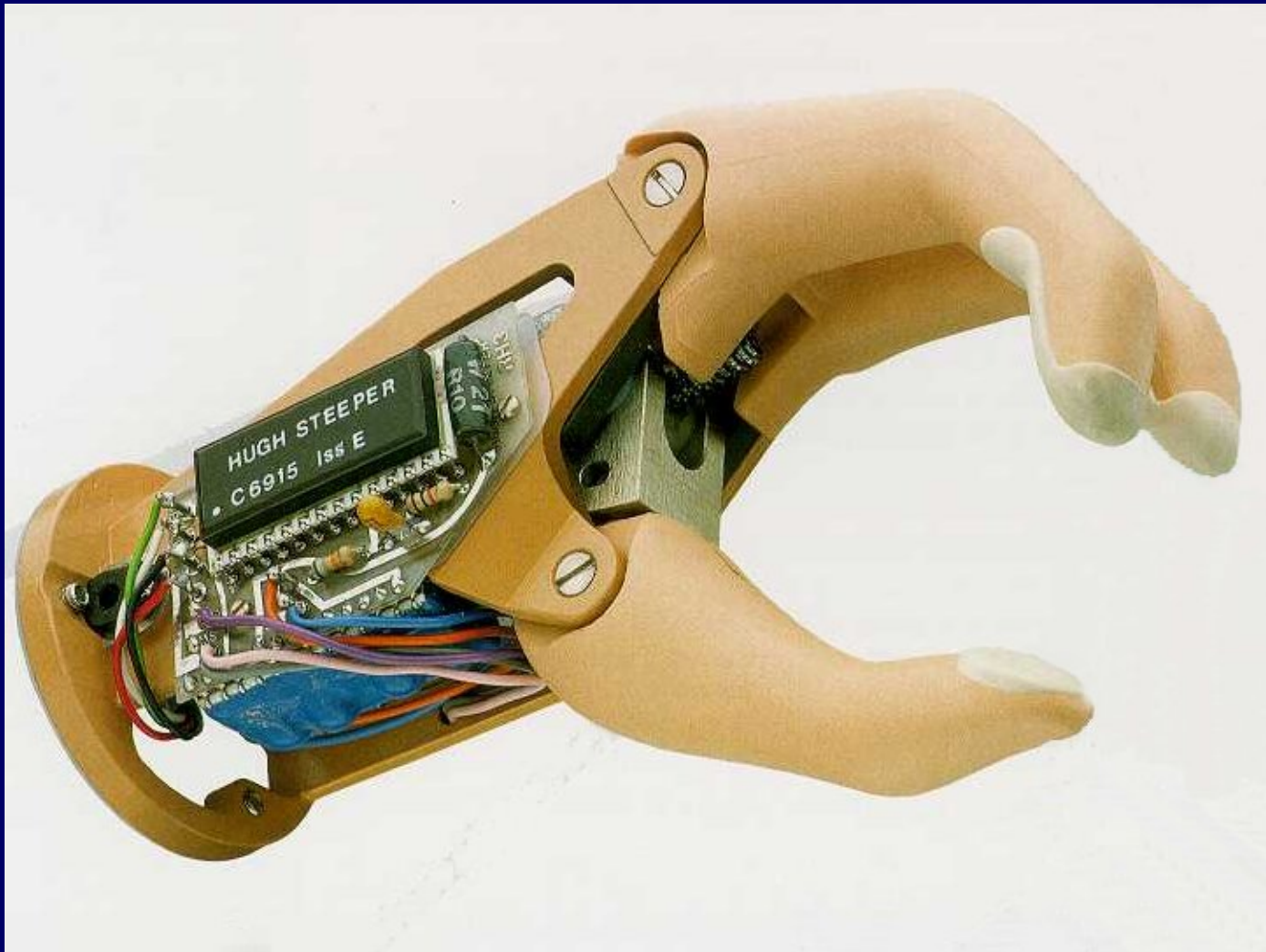


# ELECTRICAL



Otto Bock

# ELECTRICAL

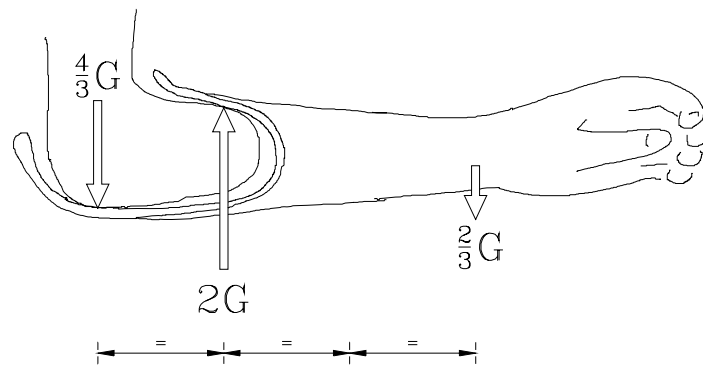
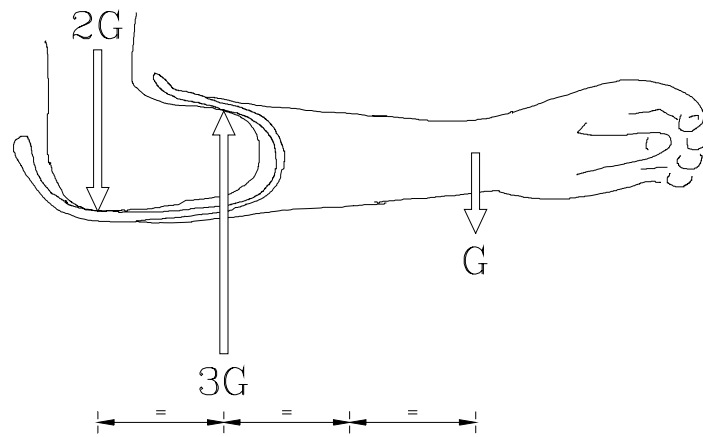


Steeper

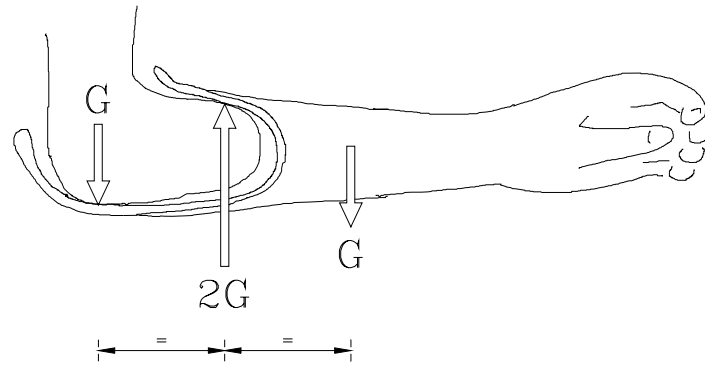
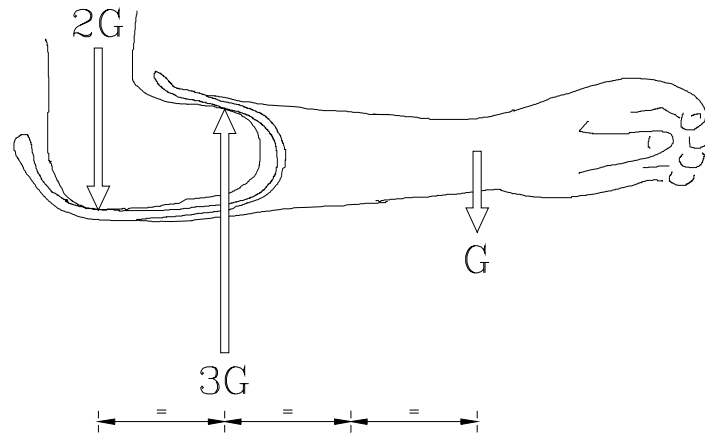
# ELECTRICAL

## DISADVANTAGES:

- HIGH MASS





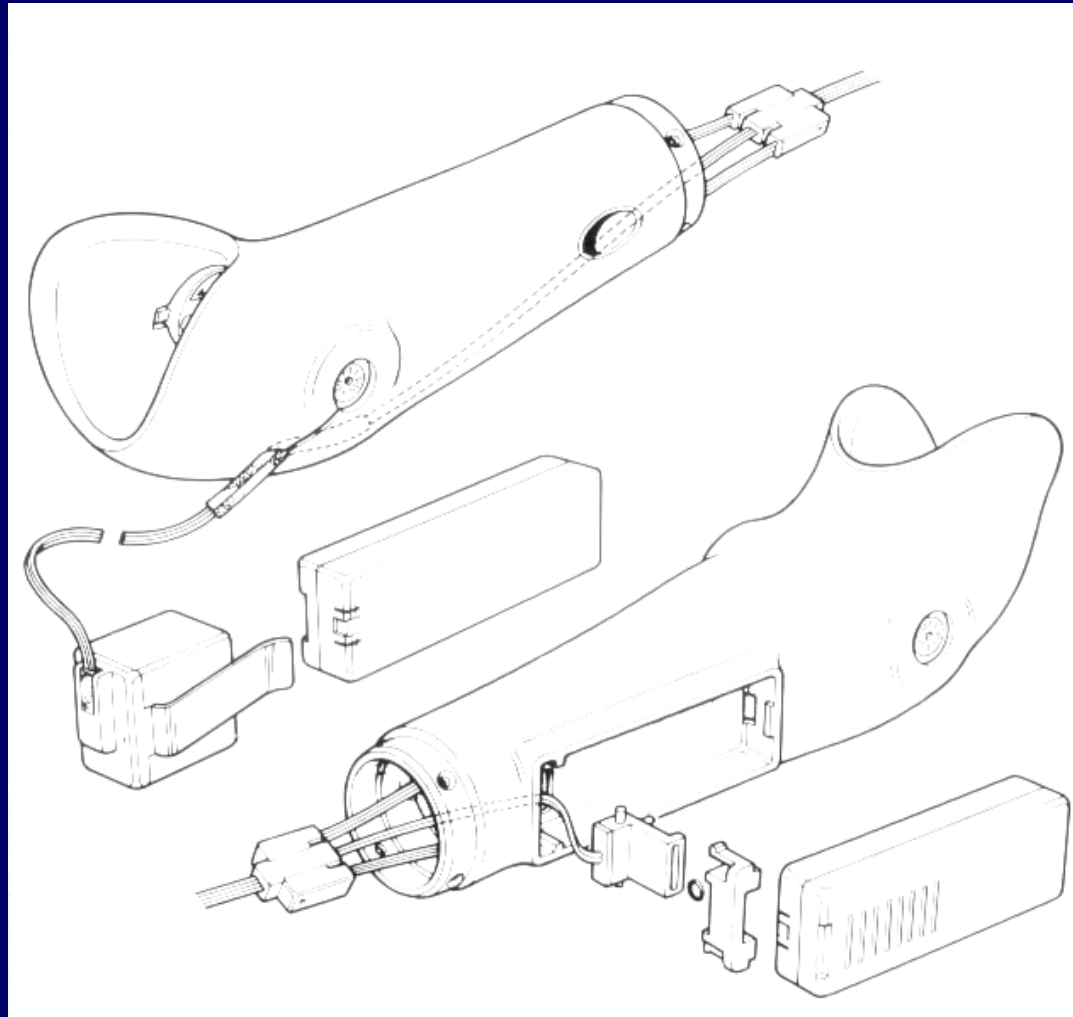


# ELECTRICAL

## DISADVANTAGES:

- HIGH MASS
- LOW SPEED
- VULNERABLE
- SIZE

# ELECTRICAL



Steeper

# HYDRAULICAL

## ADVANTAGES:

- GOOD CONTROL
- FAST
- QUIET
- NO LOCKING DEVICES NEEDED

## DISADVANTAGES:

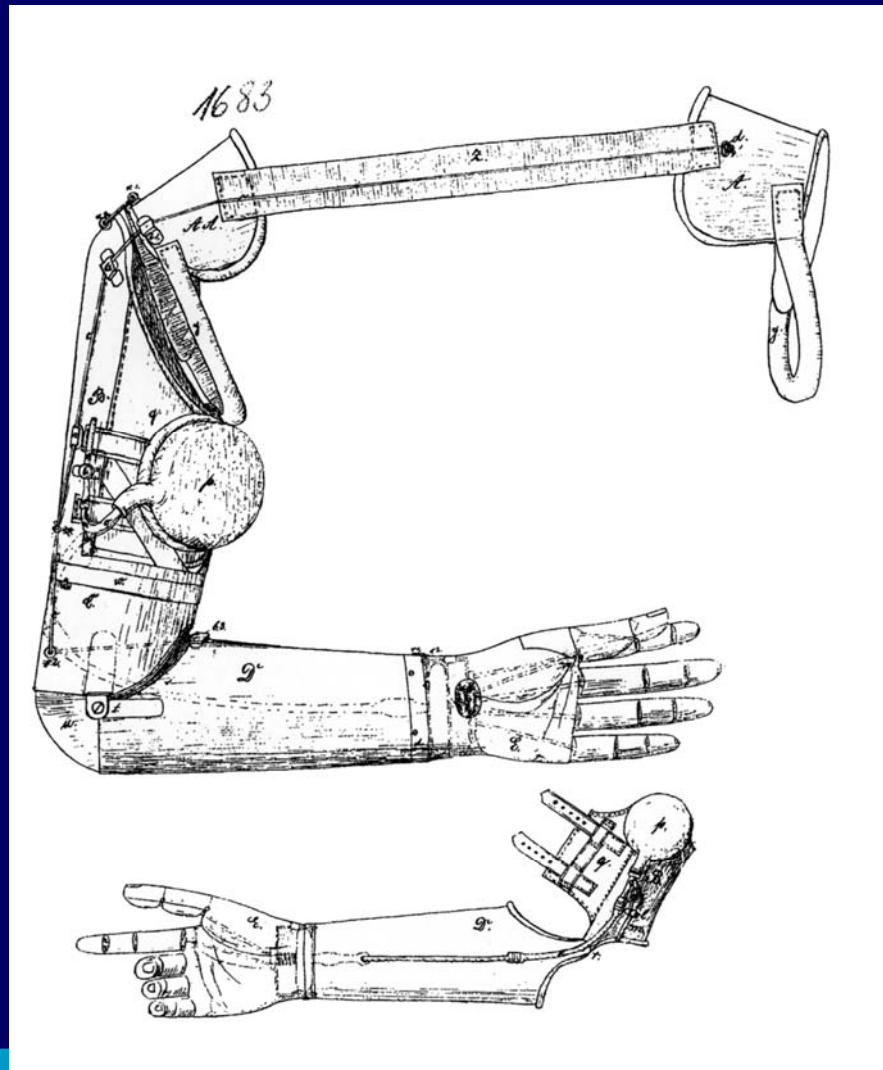
- HIGH TOTAL MASS
- LEAKAGE
- ENERGY STORAGE

# PNEUMATICAL

## ADVANTAGES:

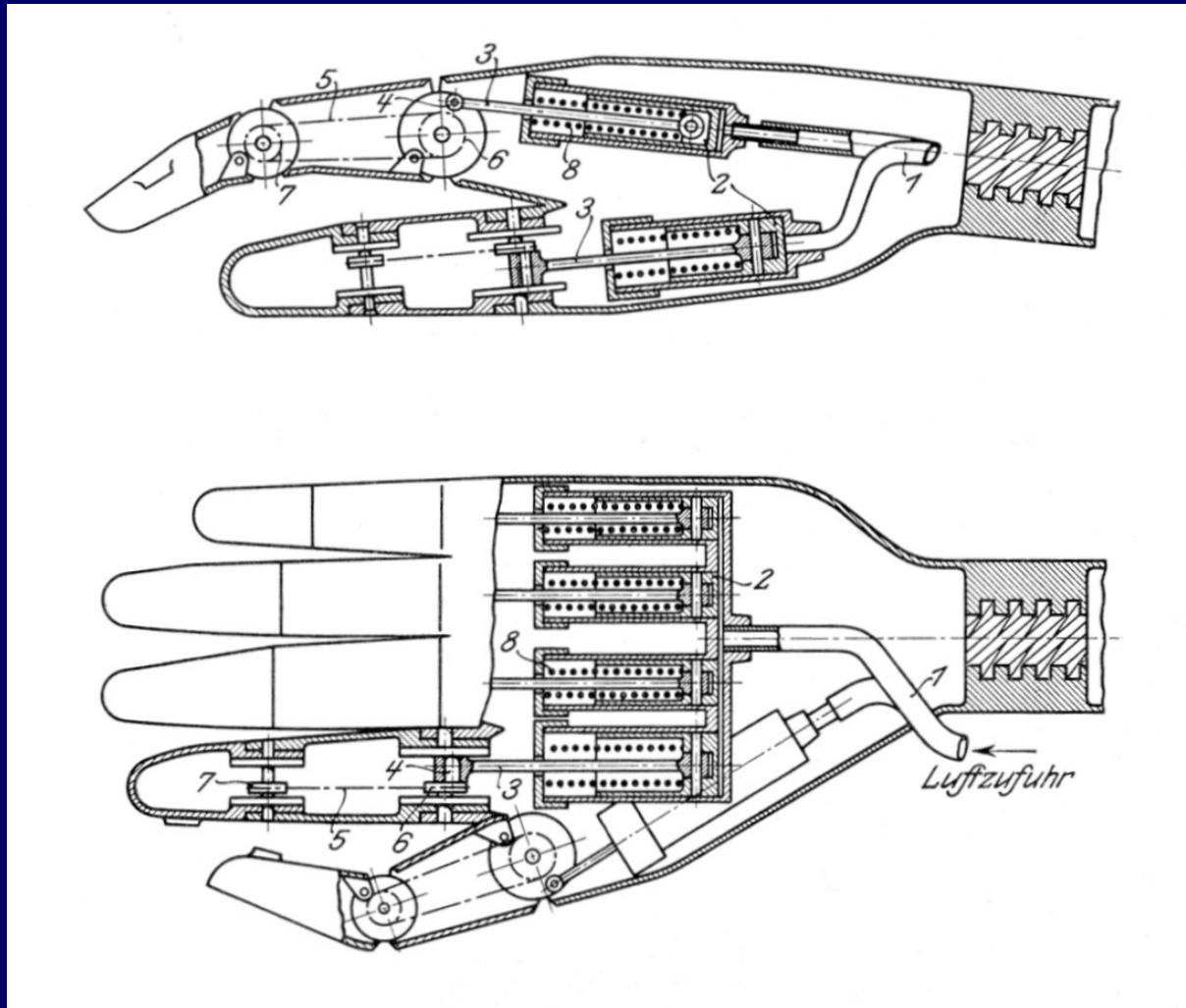
- LOW MASS
- HIGH SPEED
- RELIABLE
- SMALL

# PNEUMATICAL: DALISH 1877



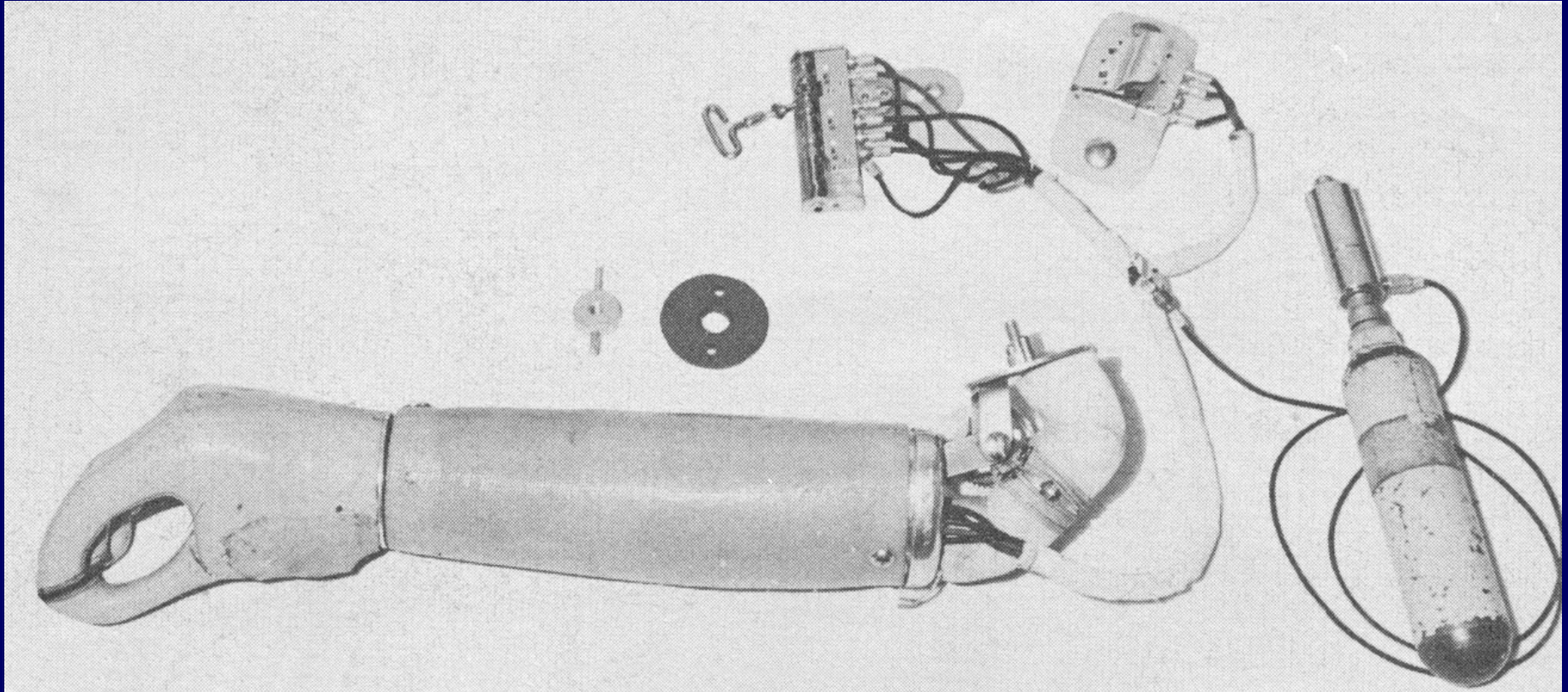
Dalish, 1877

# PNEUMATICAL: ANONYMOUS



Borchardt et al., 1919

# PNEUMATICAL: HEIDELBERG 1949+



Lucaccini, 1967

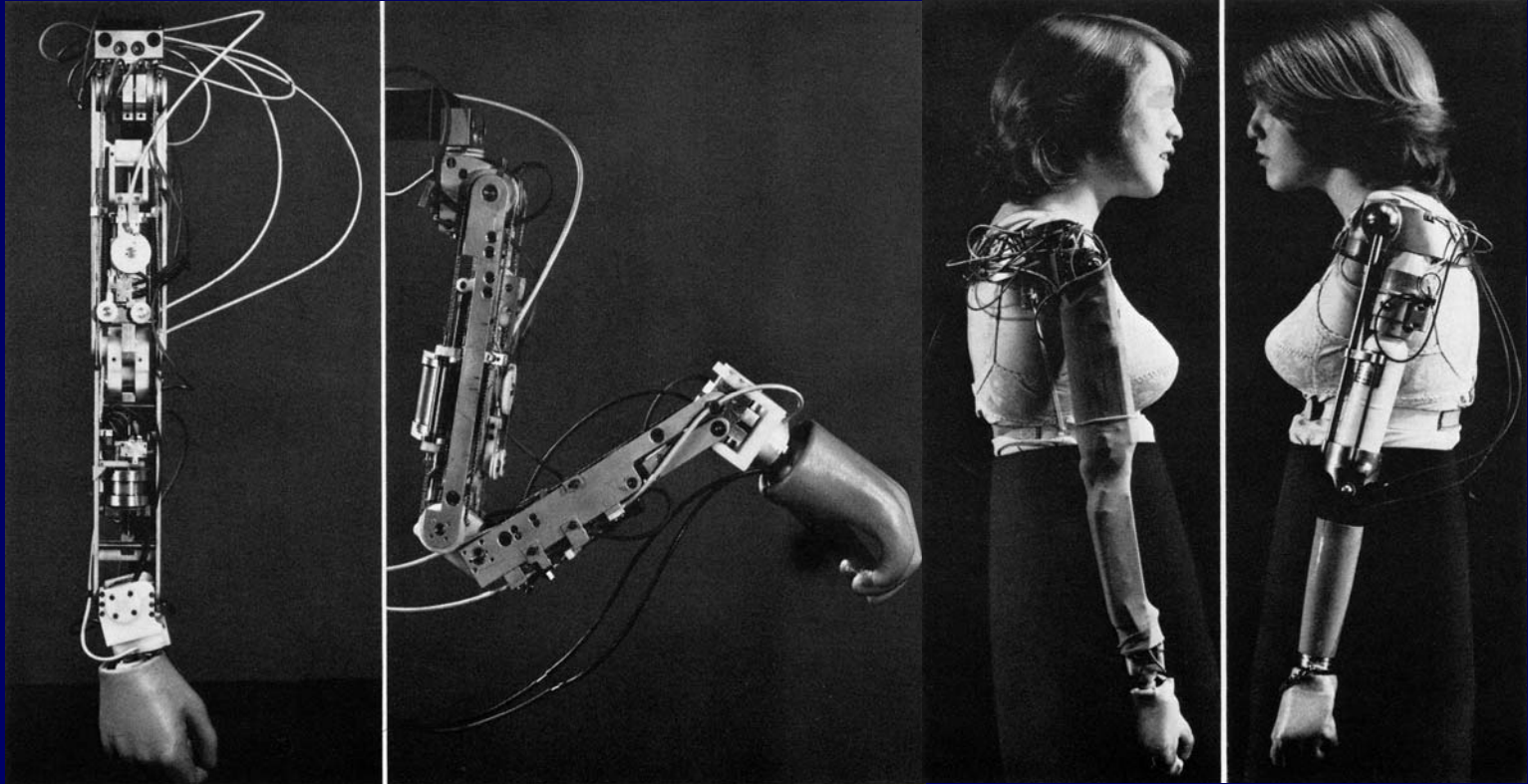


# THALIDOMIDE



Issued in 1956 by Chemie Grünenthal to fight nausea and sleeping problems in pregnant women.

# PNEUMATICAL: EDINBURGH 1963+



Baumgartner, 1977

# PNEUMATICAL: Limb Fitting Centre at Queen Mary's Hospital, Roehampton, London, 1964



nmsi  
www.nmsi.ac.uk

Steeper, 1964

# PNEUMATICAL

## DISADVANTAGES:

- HIGH OVERALL MASS
- UNRELIABLE
- HIGH GAS CONSUMPTION
- CUMBERSOME REFILL PROCEDURE

# PNEUMATICAL



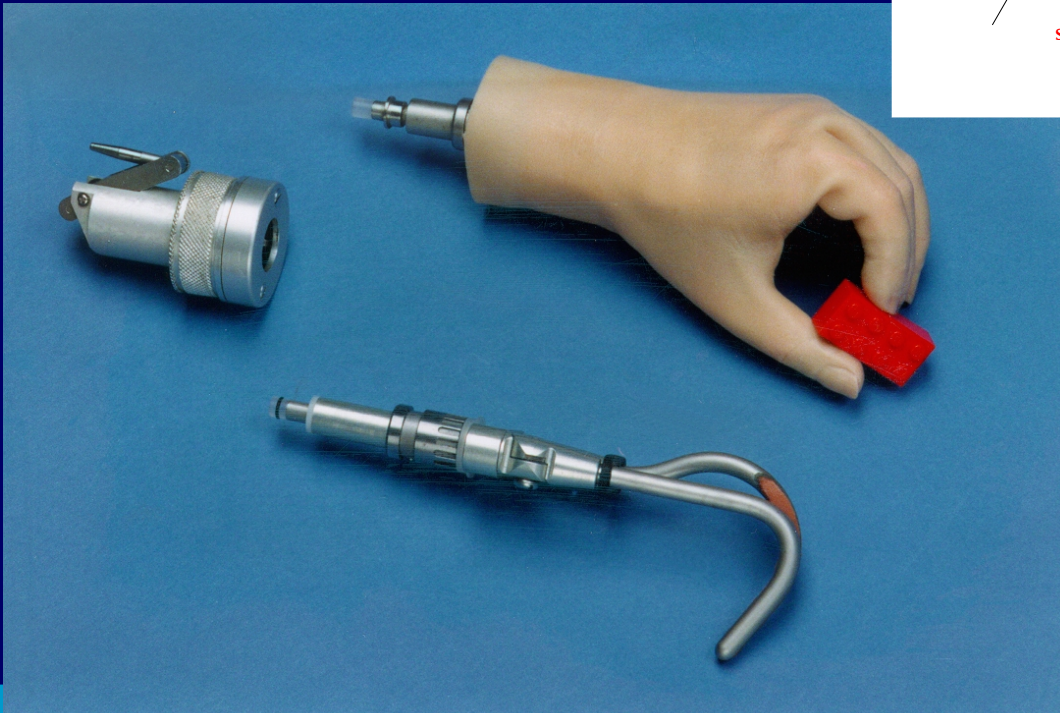
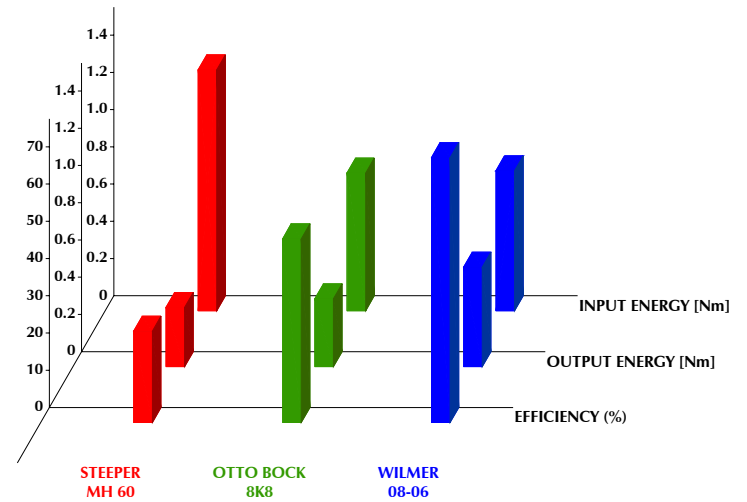
# PNEUMATICAL

## RE-ASSESSMENT PNEUMATIC ACTUATION:

- LIGHT?
- FAST?
- RELIABLE?
- SMALL?

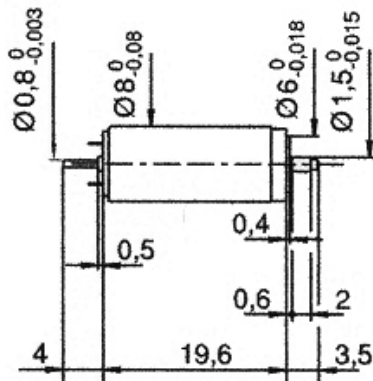
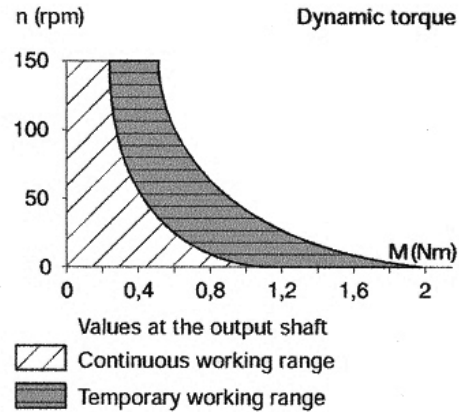
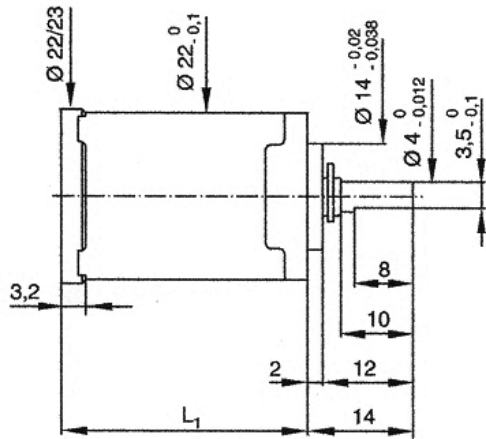


# PNEUMATICAL

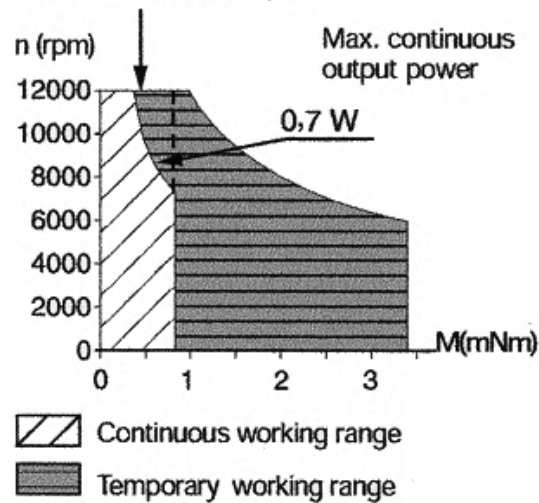


$$E_{\text{req}} = 750 \text{ Nmm}$$

# PNEUMATICAL



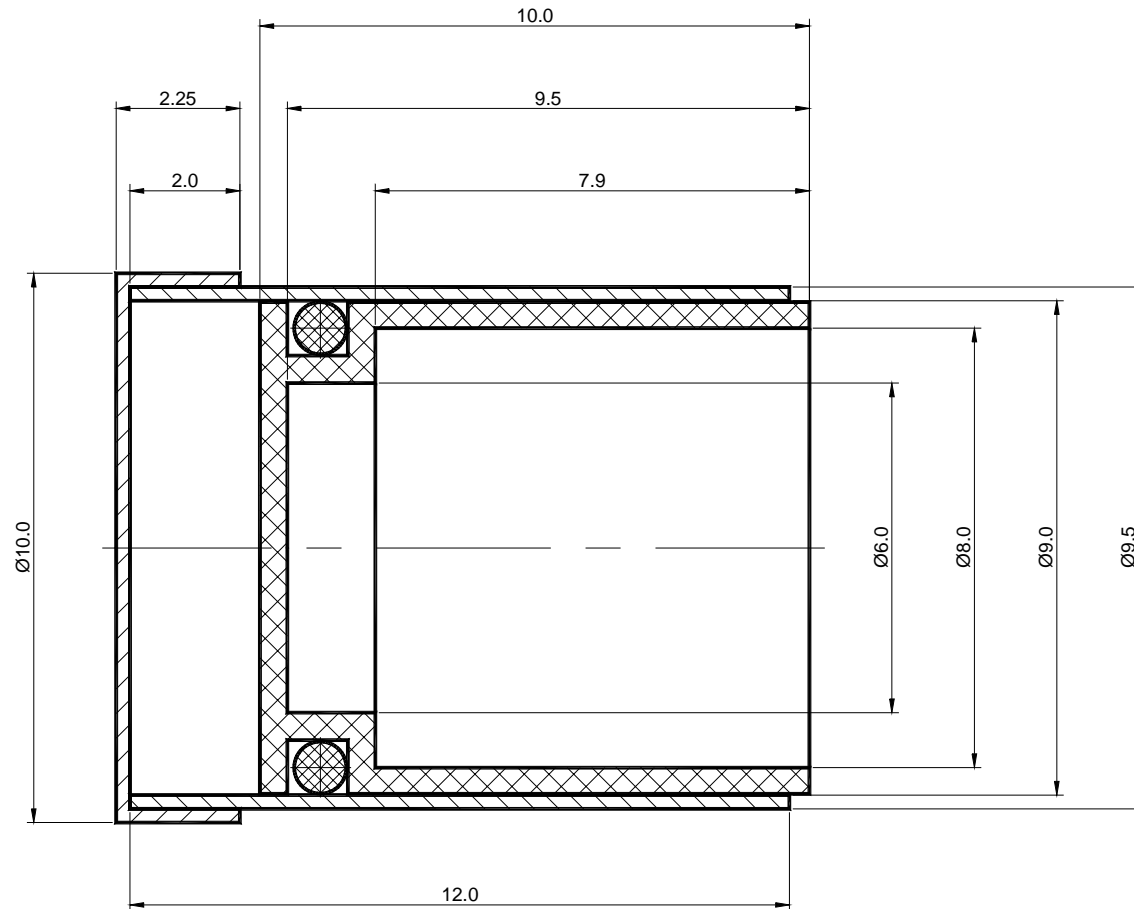
Max. recommended speed



$$m = 37.5 \text{ g}$$



# PNEUMATICAL



$m = 1.2 \text{ g}$

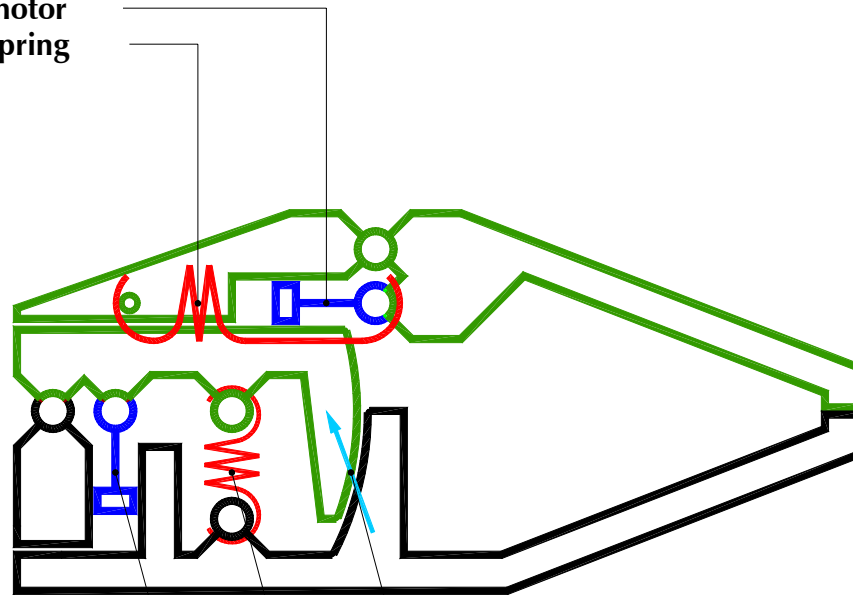
# PNEUMATICAL

- MINIMIZE GAS CONSUMPTION BY
  - SYSTEM CHOICE
  - REDUCTION OF FRICTION LOSSES
  - REDUCTION OF DEAD SPACE
  - SUPPLY PRESSURE
- PROTOTYPES

# PNEUMATICAL

## 'BI-PHASIC' OPERATION

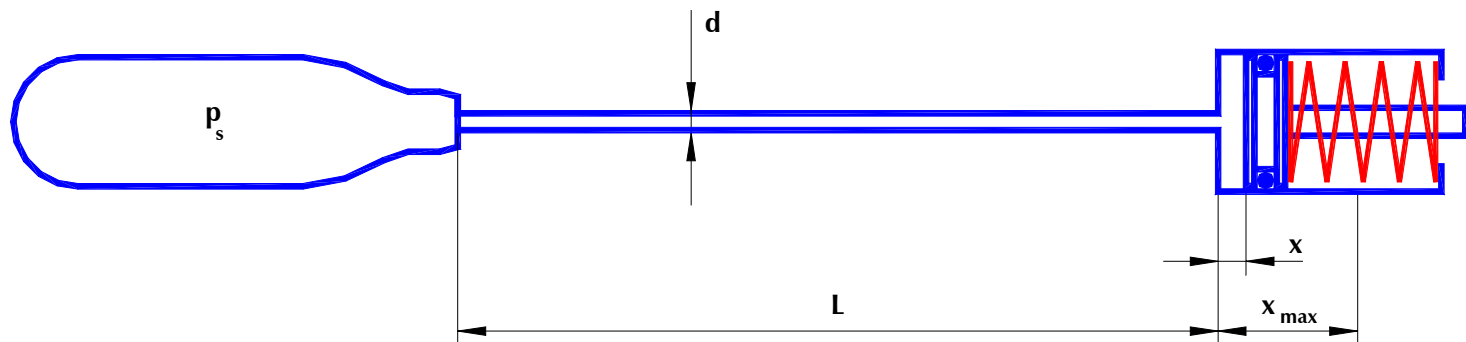
pinching motor  
pinching spring



prehension motor  
closing spring  
locking mechanism

# PNEUMATICAL

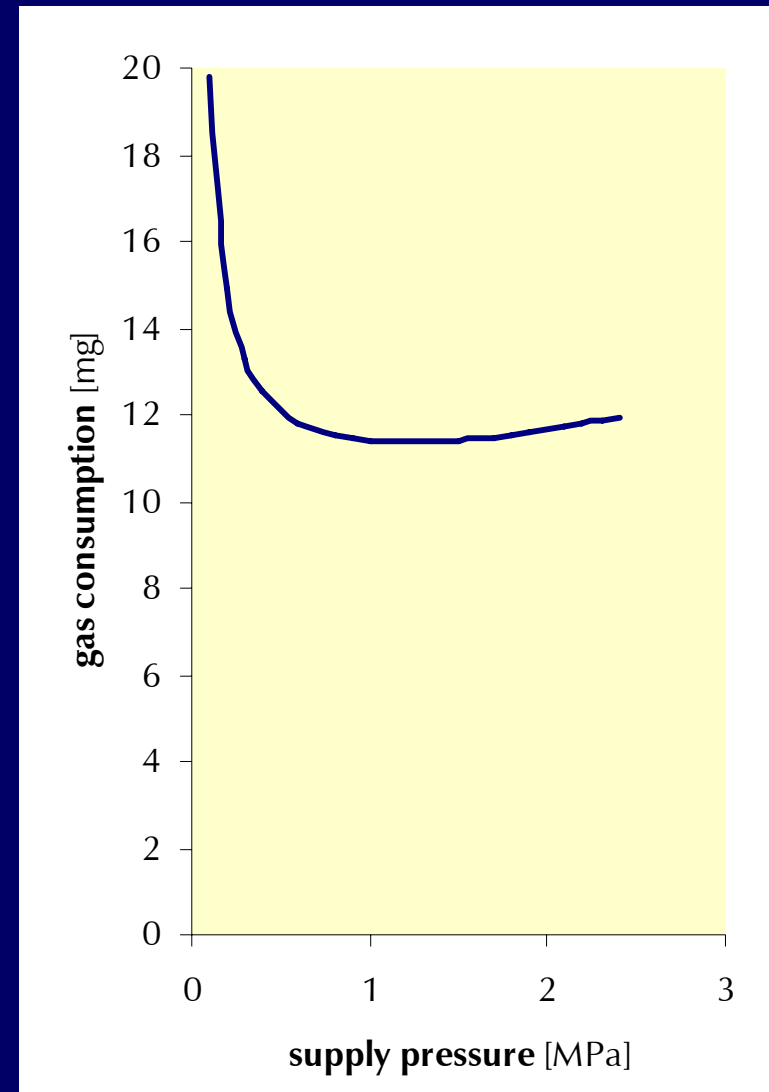
## SUPPLY PRESSURE



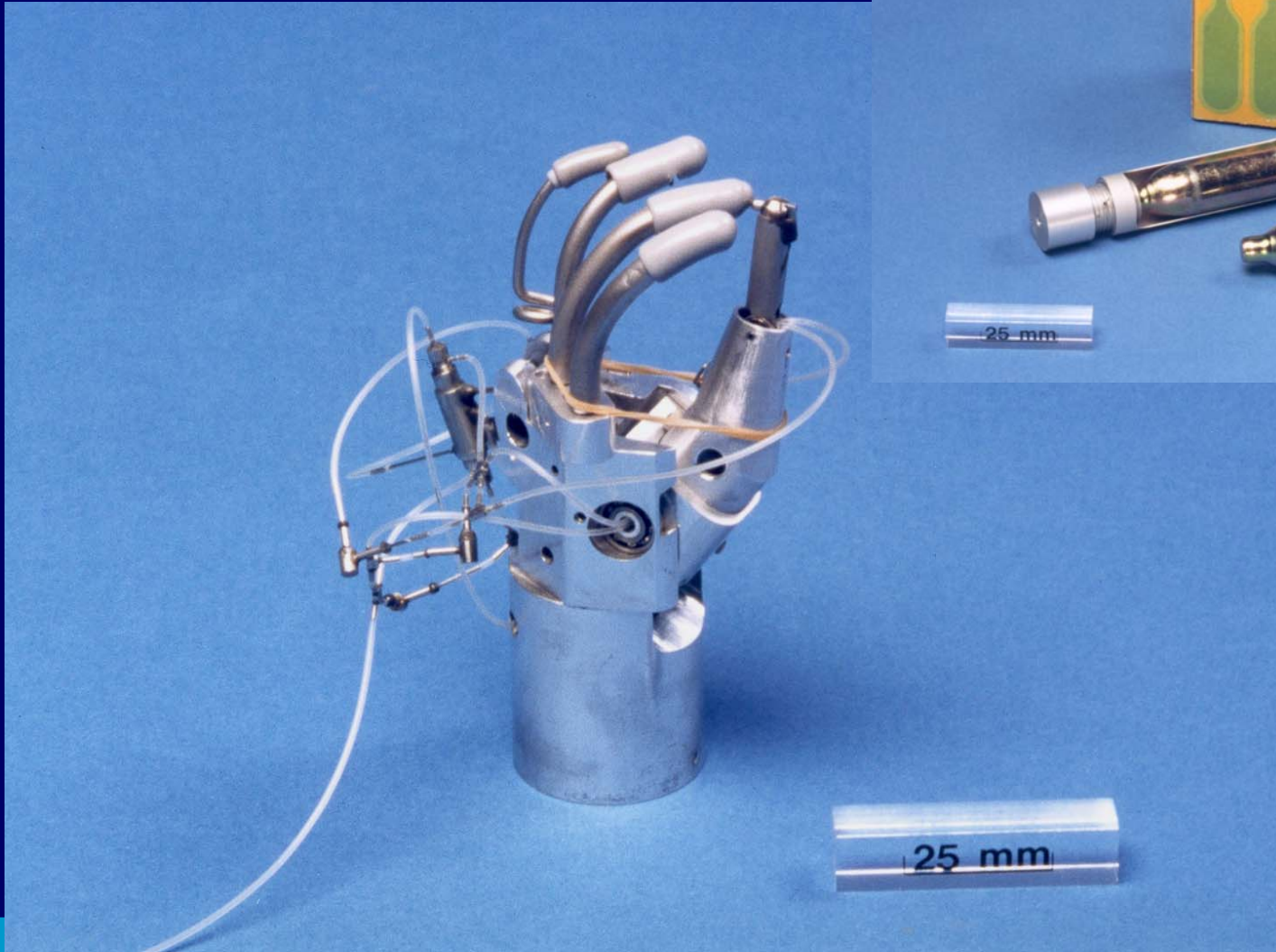
# PNEUMATICAL

$$P_{s, \text{opt}} = 1.2 \text{ MPa}$$

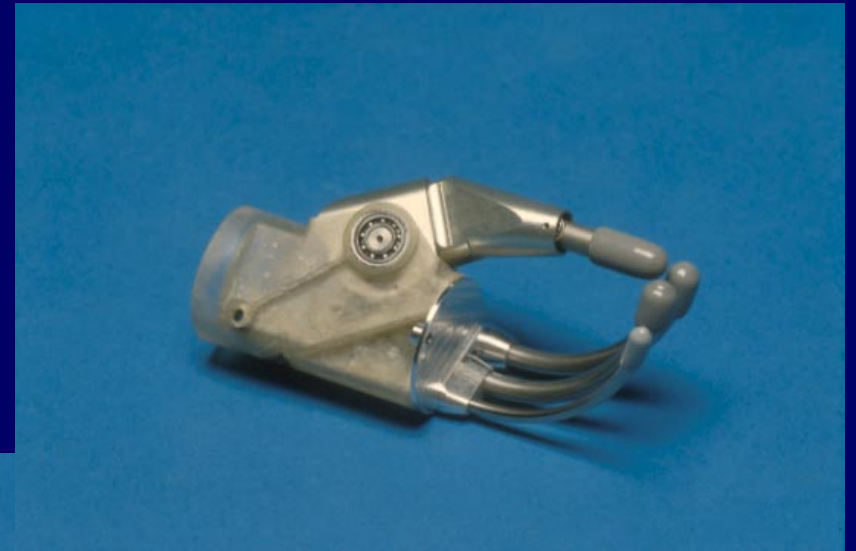
Independent of:  
 $\Delta t$ ,  $L$ ,  $F_s$ , and  $x$



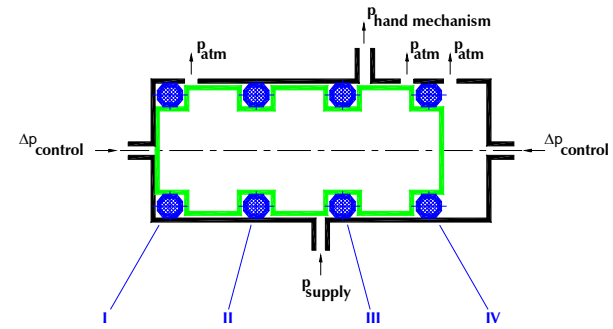
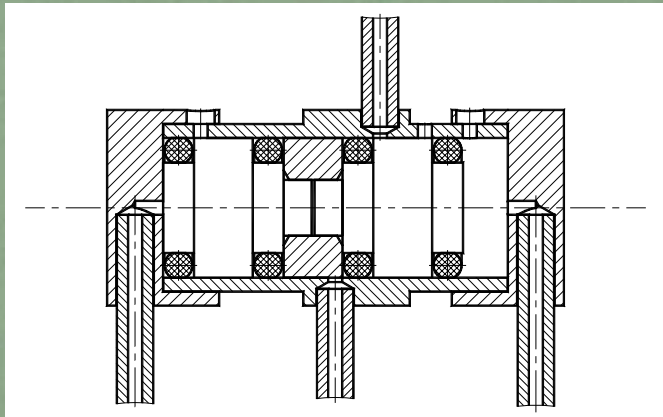
# PNEUMATICAL



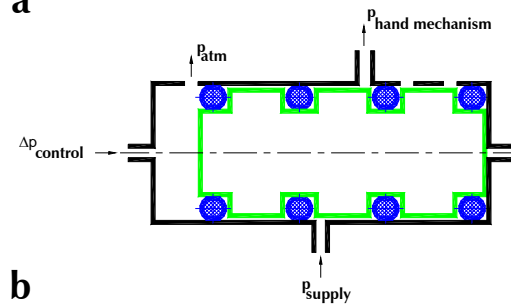
# PNEUMATICAL



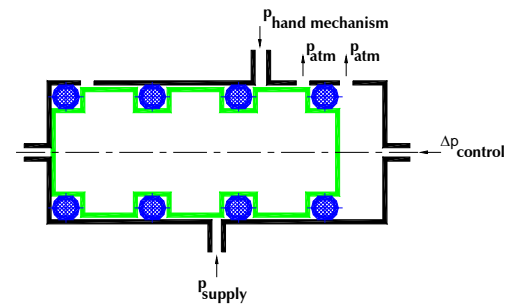
# PNEUMATICAL



a



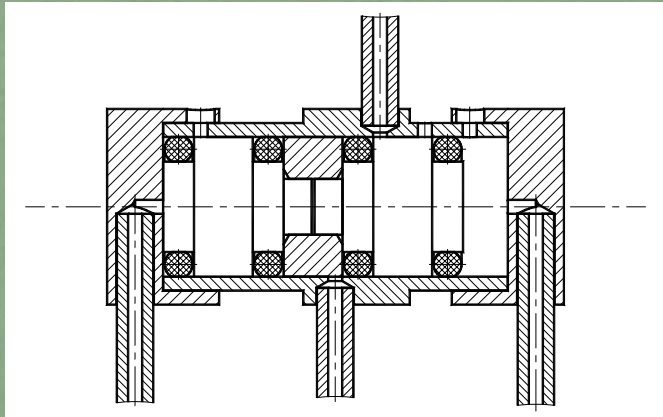
b



c



# PNEUMATICAL



Pneumatic relay:

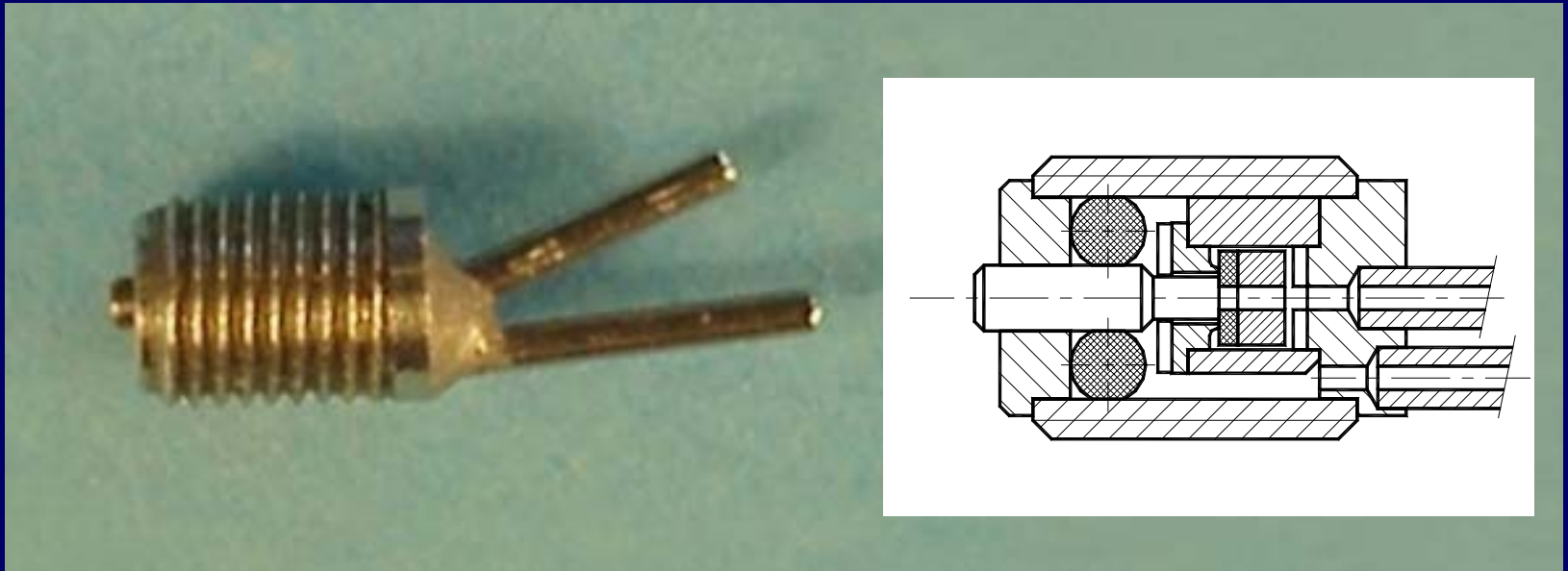
-  $\varnothing$  3.5 x 8.15 mm

-  $\Delta P = 0.4$  MPa

-  $Q = 74.2$  ltr/hr

-  $m = 0.66$  g

# PNEUMATICAL



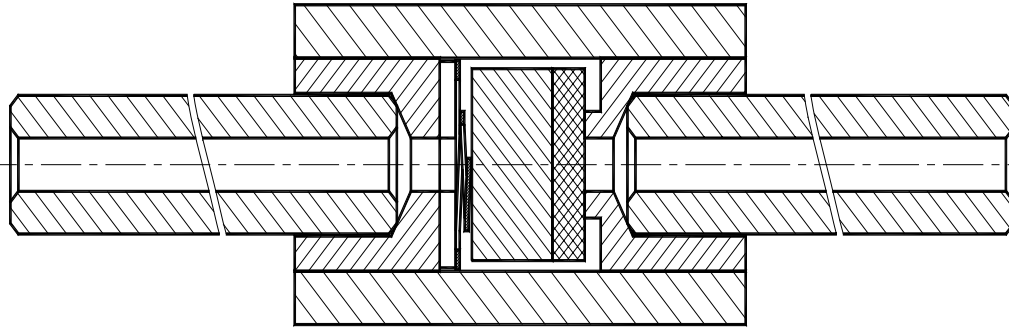
# PNEUMATICAL



Pneumatic switch:

- $\varnothing$  3.0 x 4.3 mm
- $F = 0.6$  N
- $Q = 97.0$  ltr/hr
- $m = 0.19$  g

# PNEUMATICAL



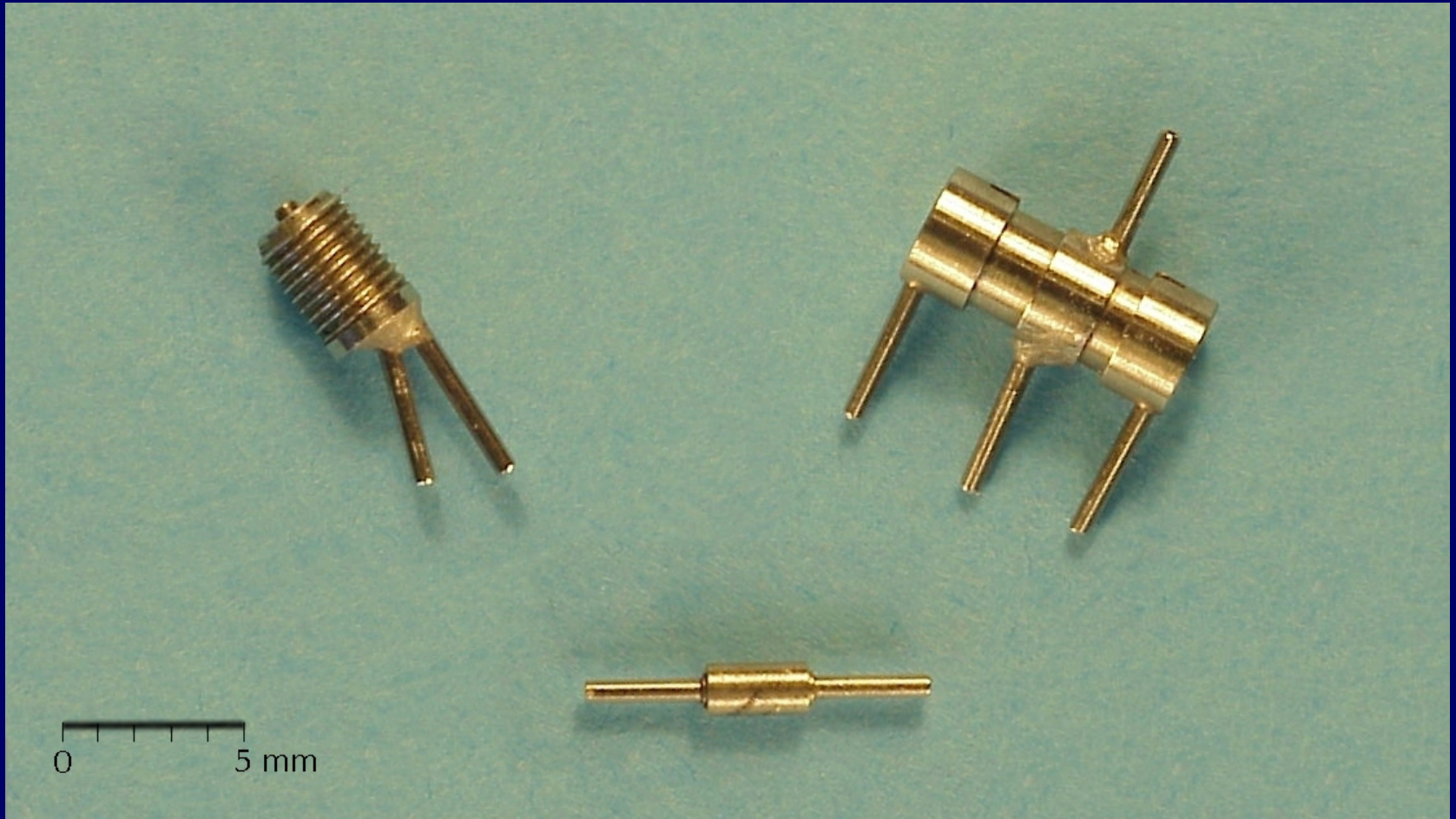
# PNEUMATICAL



Check valve:

- $\varnothing$  1.5 x 2.8 mm
- $\Delta P = 0.48$  kPa
- $Q \geq 120.0$  ltr/hr
- $m = 0.05$  g

# PNEUMATICAL





# PNEUMATICAL

	MYOELECTRIC STEEPER	MYOELECTRIC OTTO BOCK	PNEUMATIC TECHNICAL PROTOTYPE WILMER	PNEUMATIC CLINICAL PROTOTYPE WILMER
MASS OF THE HAND [grams]	230	130	128	60
MASS OF THE ENERGY STORAGE SYSTEM [grams]	75	60	60	36**
MASS OF THE COMPLETE PROSTHESIS [grams]	550	340	300*	250*
ELBOW TORQUE [Nmm]	760	470	400*	290*
ENERGY CONSUMPTION [per day]	1 BATTERY	1 BATTERY	0.5 GAS CONTAINER	< 0.5 GAS CONTAINER
OPERATING CYCLE [seconds]	2.5	>2.5	<1	<1

\* estimated figure

\*\* estimated figure, based upon a mass for the pressure reducing valve of 4 grams after a redesign

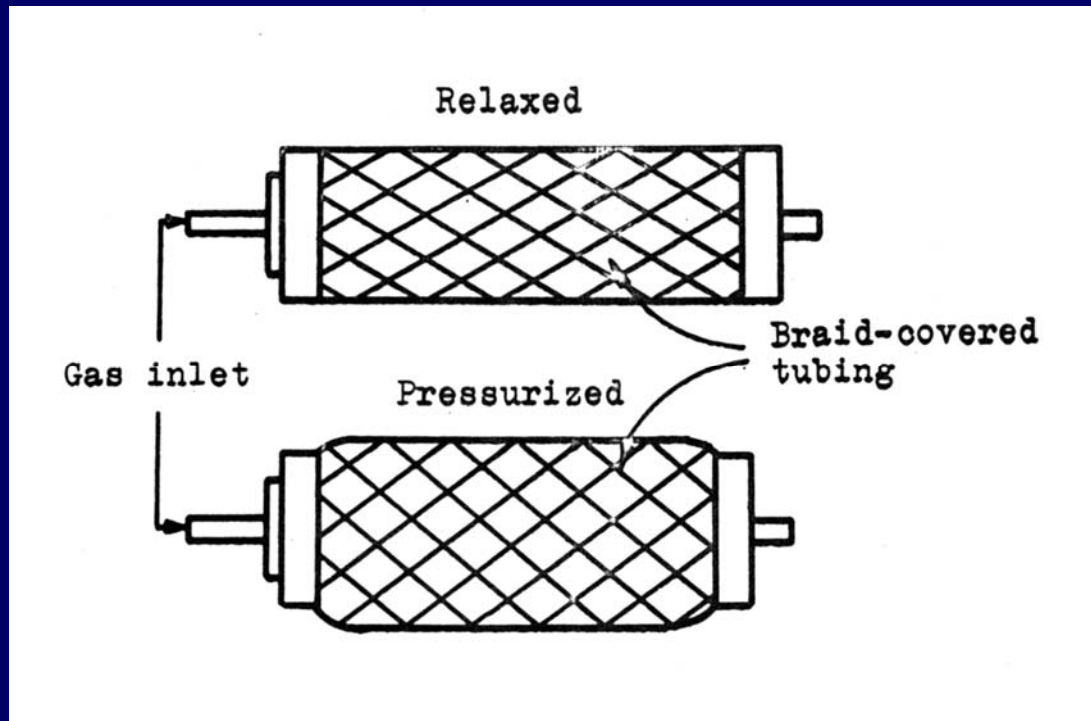
# PNEUMATICAL

## PNEUMATIC ACTUATION EXCELS ELECTRICAL ACTUATION:

- LOW IN MASS
- FAST
- RELIABLE
- SMALL



# McKIBBEN-MUSCLE



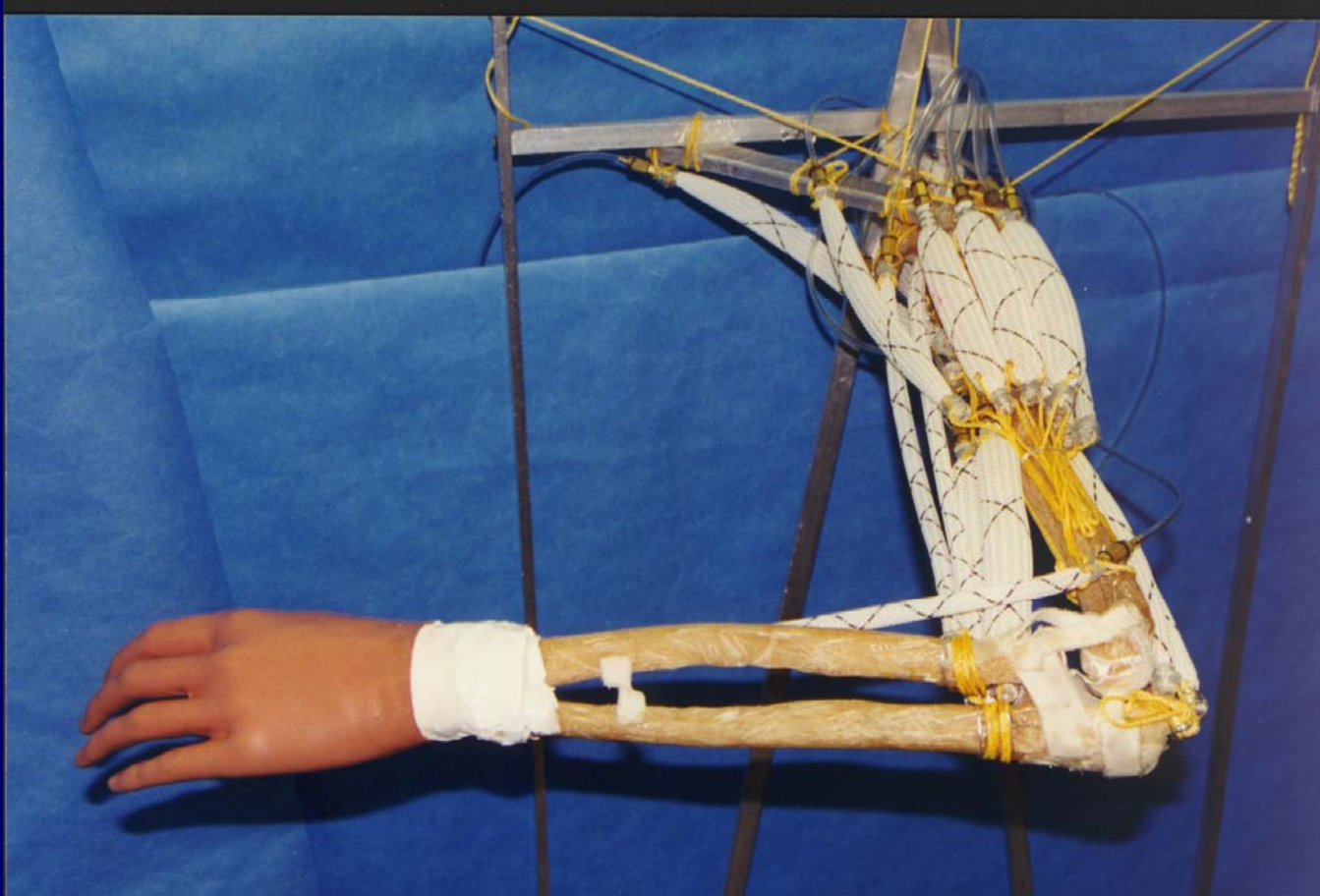
Carlson, 1971

# McKIBBEN-MUSCLE



Shadow, UK

# McKIBBEN-MUSCLE

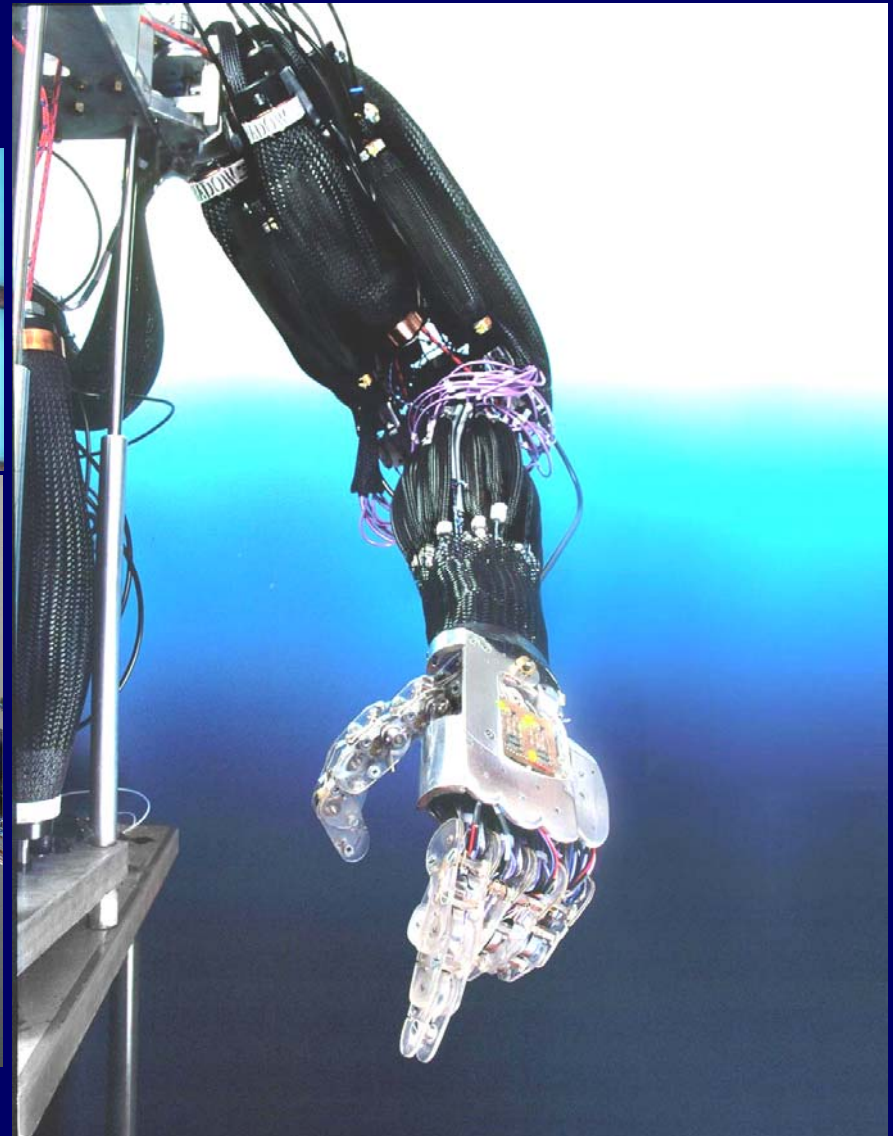


Univ. of Washington, USA

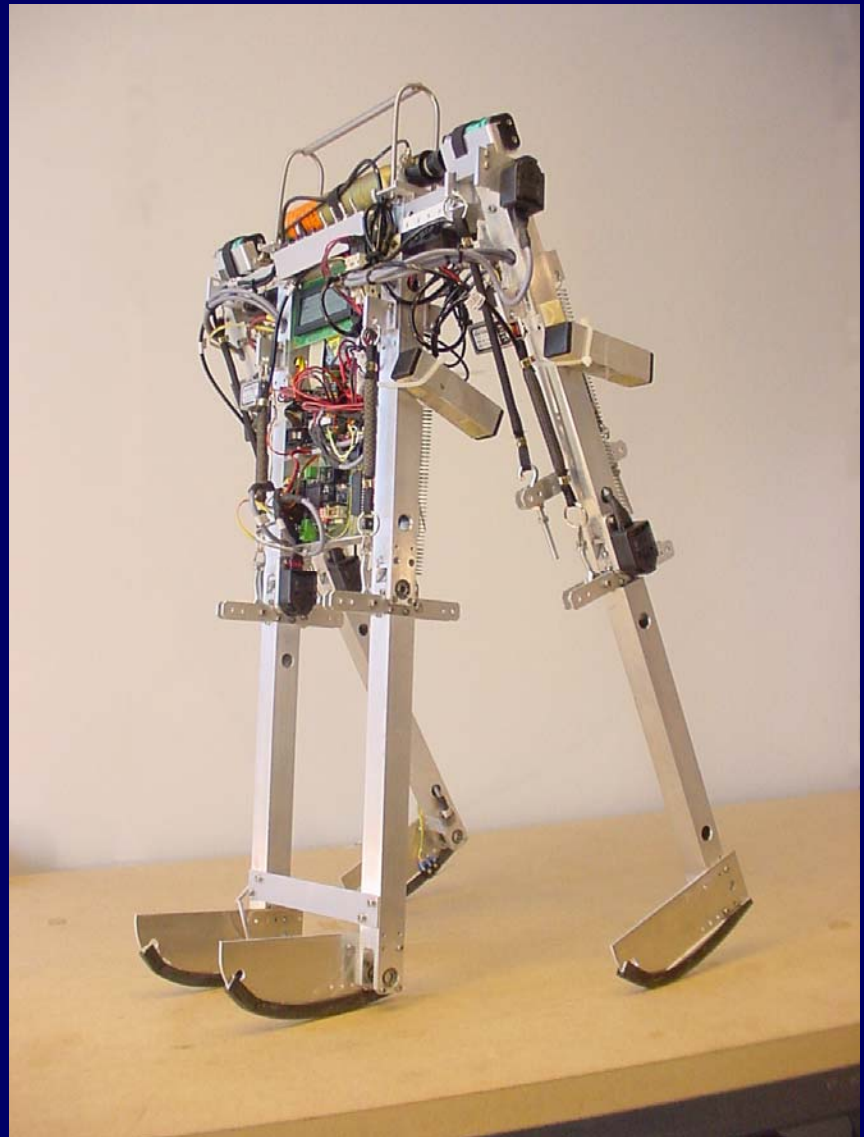
# McKIBBEN-MUSCLE



Shadow, UK



# McKIBBEN-MUSCLE





# McKIBBEN-MUSCLE



# McKIBBEN MUSCLE / PNEUMATIC ARTIFICIAL MUSCLE

## KEY ADVANTAGE:

- LOW MASS COMPARED TO MUSCLE STRENGTH
- HIGH FORCE TO WEIGHT RATIO
- HIGH POWER TO WEIGHT RATIO
- ETC.



# McKIBBEN-MUSCLE / PNEUMATIC ARTIFICIAL MUSCLE

## CLAIMED ADVANTAGES:

- LOW MASS
- HIGH POWER-TO-WEIGHT RATIO



## DISADVANTAGES:

- LOW PRESSURE
- UV-SENSITIVE



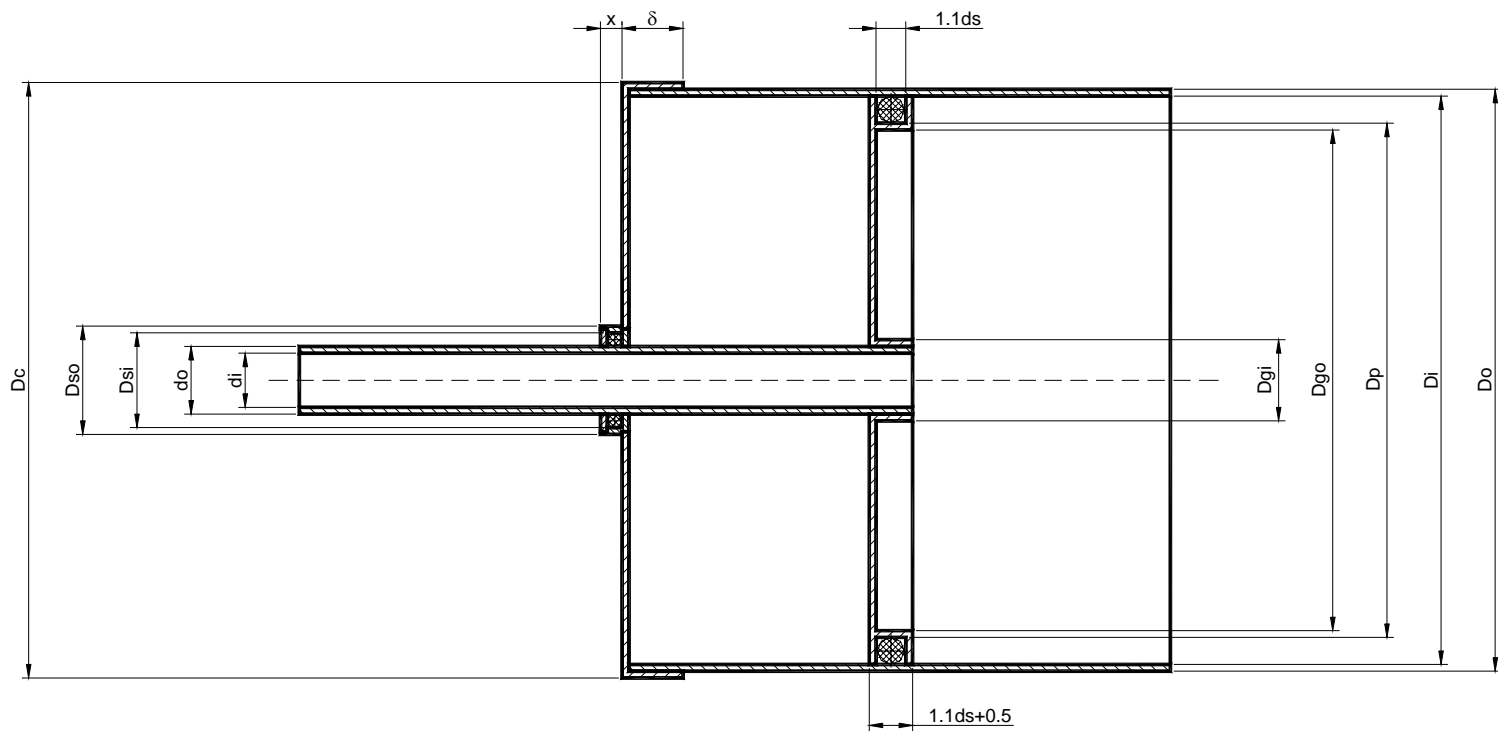
Festo AG



FESTO MAS-10

FESTO ADVC-25

FESTO DSN-25



WILMER 21xS

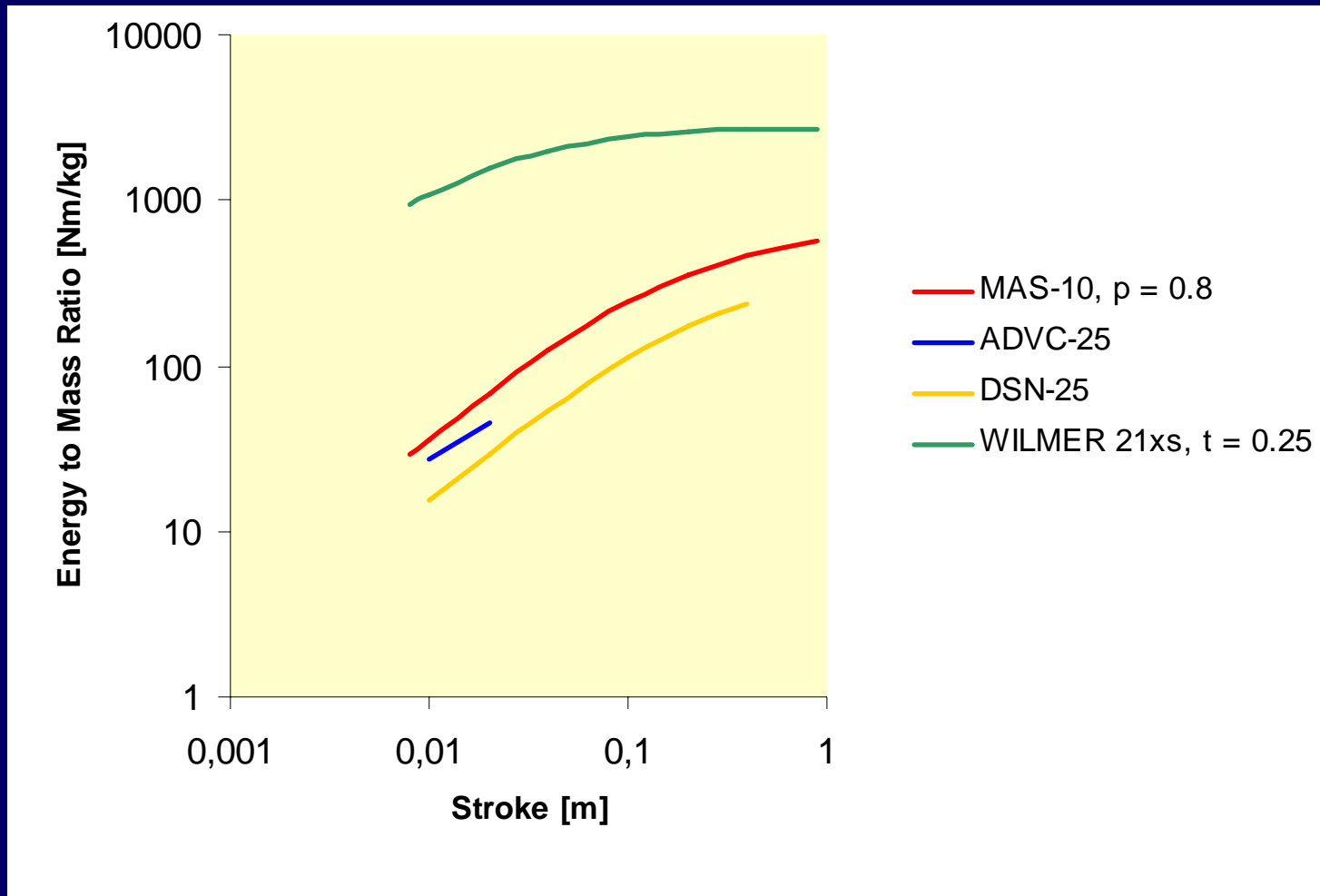
# PNEUMATIC ARTIFICIAL MUSCLES

Output energy to mass ratio:

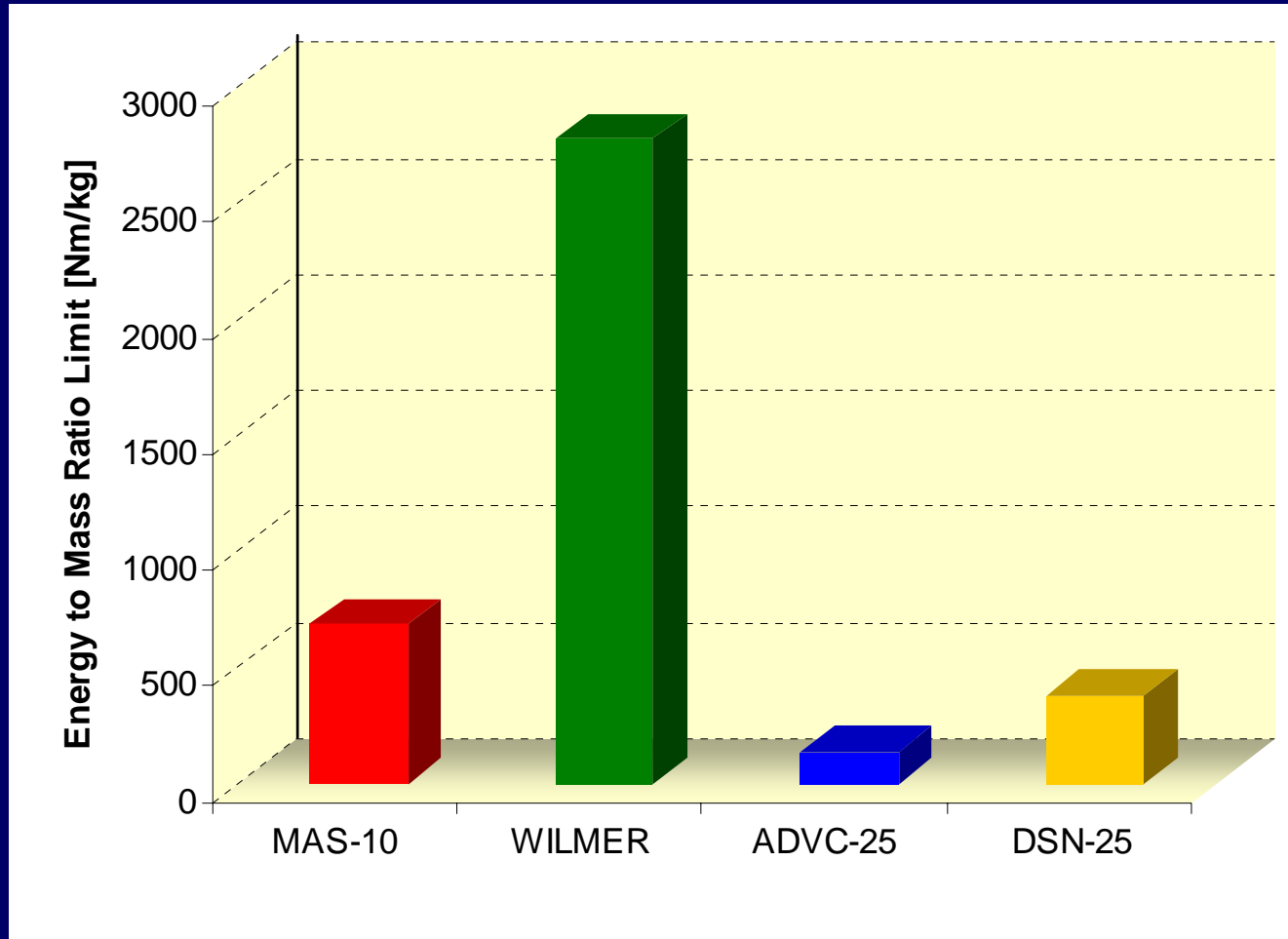
$$EtM = \frac{\int F(s) \cdot ds}{m}$$

- EtM = energy to mass ratio [Nm/kg]
- F(s) = output force as a function of the stroke [N]
- s = stroke [m]
- m = muscle mass [kg]

# PNEUMATIC ARTIFICIAL MUSCLES



# PNEUMATIC ARTIFICIAL MUSCLES





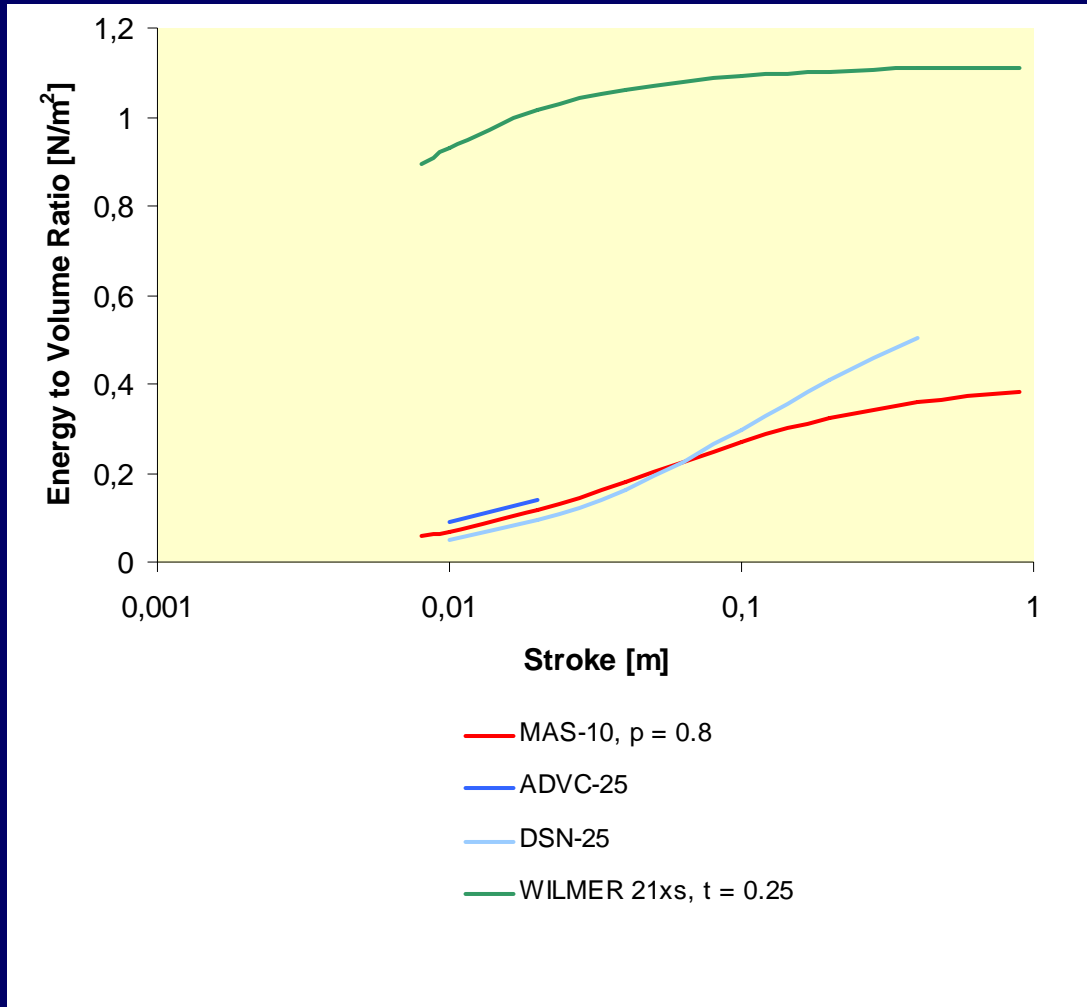
# PNEUMATIC ARTIFICIAL MUSCLES

Output energy to volume ratio:

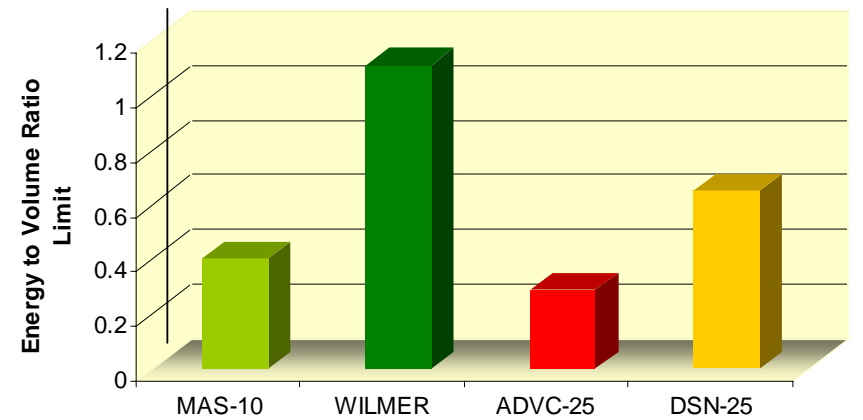
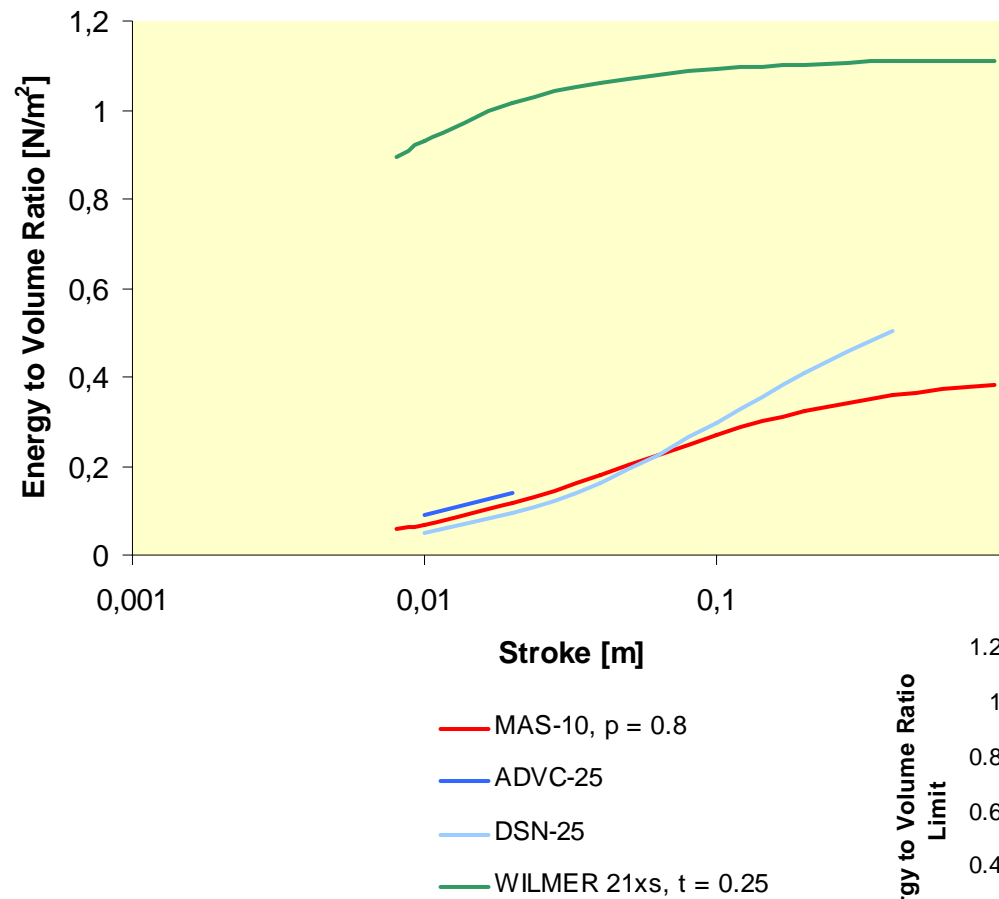
$$EtV = \frac{\int F(s) \cdot ds}{V}$$

- $EtV$  = energy to mass ratio [Nm/kg]
- $F(s)$  = output force as a function of the stroke [N]
- $s$  = stroke [m]
- $V$  = muscle volume [m<sup>3</sup>]

# PNEUMATIC ARTIFICIAL MUSCLES



# PNEUMATIC ARTIFICIAL MUSCLES



# PNEUMATIC ARTIFICIAL MUSCLES

Festo MAS



Festo DMSP

# PNEUMATIC ARTIFICIAL MUSCLES

Festo MAS



Festo DMSP

Basic mass difference

$$\Delta m = 20 \text{ g}$$

# PNEUMATIC ARTIFICIAL MUSCLES

## CONCLUSIONS:

$$(EtM)_{PAM} > (EtM)_{\text{Standard Industrial Actuators}}$$

$$(EtV)_{PAM} < (EtV)_{\text{Standard Industrial Actuators}}$$

## REDESIGN OF CYLINDER ACTUATORS:

$$EtM: 5 - 30 \times (EtM)_{PAM}$$

$$EtV > 3 - 13.5 \times (EtV)_{PAM}$$

**DO NOT USE PAM WHERE EtM  
AND/OR EtV IS CRITICAL**

# SUMMARY

- CONTROL vs ACTUATION
- BODY POWER
  - SHOULDER HARNESS
  - ELBOW CONTROL
- EXTERNAL POWER
  - ELECTRICAL
  - HYDRAULICAL
  - PNEUMATICAL

# SUMMARY [cont.]

- PNEUMATIC ACTUATION EXCELS ELECTRICAL ACTUATION:
  - LOW IN MASS
  - FAST
  - RELIABLE
  - SMALL
- DO NOT USE PAM WHERE  $E_tM$  AND/OR  $E_tV$  IS CRITICAL



## CHALLENGES IN PNEUMATICS:

Miniature and energy efficient pneumatical systems

### Research at the Delft Institute of Pneumatics:

- Miniature components
- [Energy efficient] pressure supply
- Miniature servo mechanisms

# Pneumatics

## - miniature components

**WILMER**  
ADVANCED MEDICAL TECHNOLOGY

**TU Delft**

Delft University of Technology

Mechanical Engineering  
Man Machine Systems  
WILMER prosthetics laboratory

Address  
Mekelweg 2  
2628 CD Delft  
The Netherlands

<http://mms.tudelft.nl/wilmer>



2004

### MASTER GRADUATION PROJECT

### DESIGN OF A MINIATURE PRESSURE REGULATOR

Autonomous systems, like hand prostheses and walking bipeds, are to be powered by pneumatic actuators for reasons of overall mass, speed, reliability, and size. With the proper system choice made, a relatively small gas container holds sufficient energy to power the system during its duty cycle. In the container the gas is stored at saturation pressure. In general the saturation pressure level does not correspond with energy efficient operation of the system. Therefore, a pressure regulator is needed to reduce the saturation pressure to the desired supply pressure for the system. Pressure regulators are available from many different commercial firms. These regulators are all characterized by a relatively large size and mass. Although several prototypes of pressure regulators have been made at MMS that are small compared to the commercially available regulators, they are still large compared to other system components in hand prostheses and/or walking bipeds.

### ASSIGNMENT

Design, construct, and build a miniature pressure regulator. Typical dimensions:  $\varnothing 5 \times 25$  mm. Pressure range: 0.35 – 1.5 MPa. Output flow > 20 ltr/hr. Demonstrate the proper working order of the new design in an experimental setup.

### ADDITIONAL INFORMATION:

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# Pneumatics

- miniature components

Pressure regulation in the human eye  
[treatment of glaucoma]

Project in co-operation with



&



Rotterdam Eye Hospital

# Pneumatics

## - supply pressure level

**WILMER**  
ADVANCED MEDICAL TECHNOLOGY

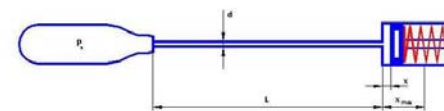
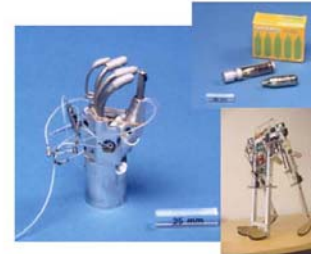
**TU Delft**

Delft University of Technology

Mechanical Engineering  
Man Machine Systems  
WILMER prosthetics laboratory

Address  
Mekelweg 2  
2628 CD Delft  
The Netherlands

<http://mms.tudelft.nl/wilmer>



2004

### MASTER GRADUATION PROJECT

### OPTIMAL SUPPLY PRESSURE LEVEL

For autonomous and/or portable systems, like for instance hand prostheses or walking bipeds, pneumatic actuation is designated. For the energy supply pressurized carbon dioxide is used, and stored at its saturation pressure [5.7 MPa]. Previously performed theoretical analysis, based upon a isothermal approach, combined with limited experimental data, suggest the amount of gas used for an operating cycle of the system is at its minimum if the saturation pressure is reduced to a supply pressure level of 1.2 MPa. To further support this outcome additional theoretical analysis based upon an adiabatic and/or a polytropic approach is required, whereas additional experiments need to verify the theoretical results.

#### ASSIGNMENT

Examine the optimal supply pressure level by a theoretical analysis based upon an adiabatic and/or a polytropic approach.  
Design, construct, and build an experimental setup for the verification of the theoretical analysis.  
Execute the experiments.

#### ADDITIONAL INFORMATION:

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# Pneumatics

- exergy saving

**WILMER**  
ADVANCED MEDICAL TECHNOLOGY

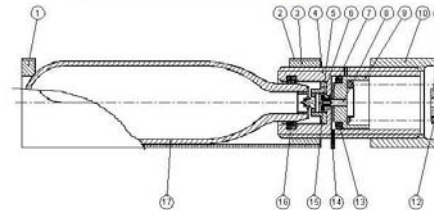
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2004

**MASTER GRADUATION PROJECT**

## **EXERGY SAVING PNEUMATIC SYSTEMS**

For autonomous and/or portable systems, like for instance hand prostheses or walking bipeds, pneumatic actuation is designated. For the energy supply pressurized carbon dioxide is used, and stored at its saturation pressure [5.7 MPa]. Previously performed theoretical analysis, based upon a isothermal approach, combined with limited experimental data, suggest the amount of gas used for an operating cycle of the system is at its minimum if the saturation pressure is reduced to a supply pressure level of 1.2 MPa. Yet, in reducing the gas pressure from 5.7 to 1.2 MPa a lot of potential energy [exergy] originally stored in the gas at saturation pressure is wasted.

### **ASSIGNMENT**

Investigate possible ways to utilize more of the potential energy of carbon dioxide stored at saturation pressure. Design, construct, and build an experiment based upon one of these options and prove the energy savings.

### **ADDITIONAL INFORMATION:**

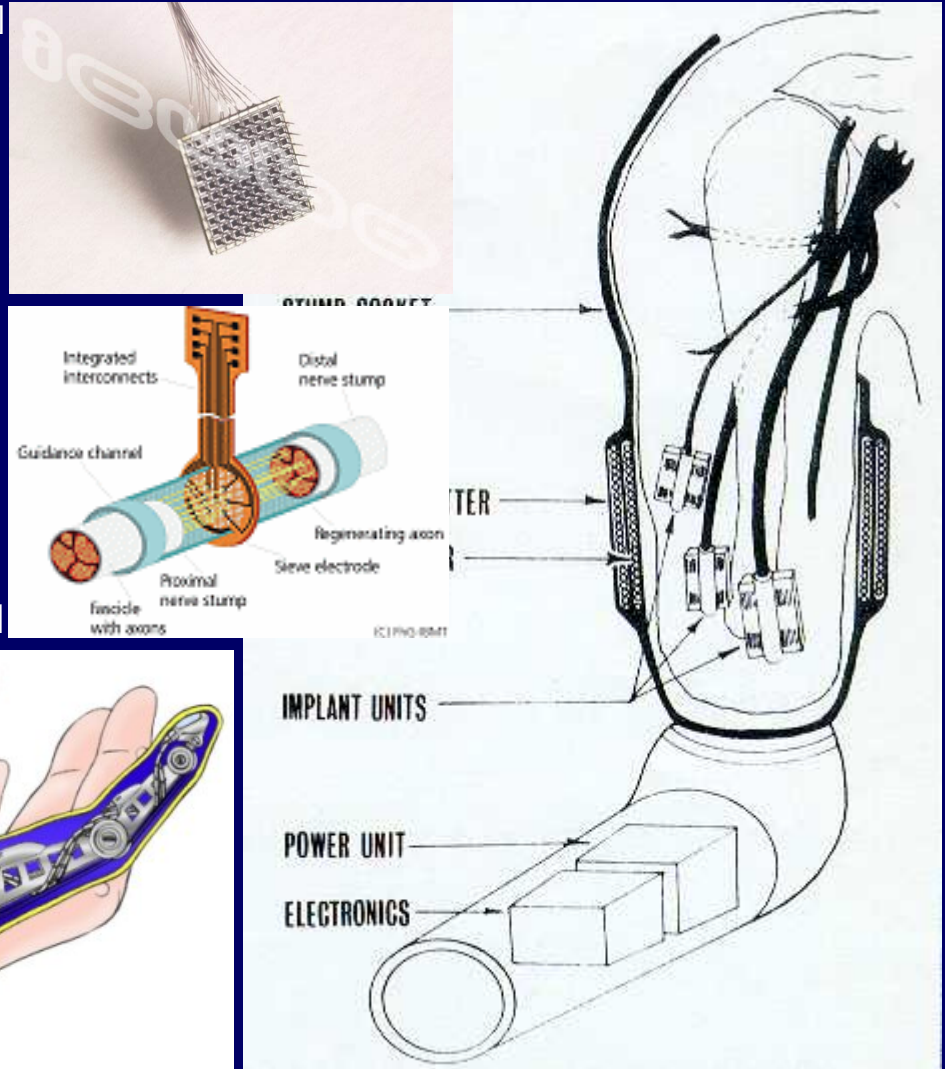
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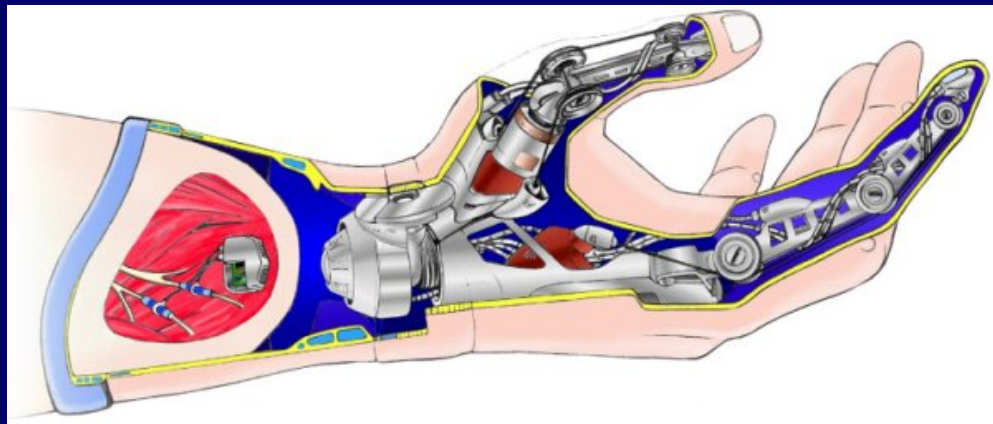
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# Pneumatics

- servo mechanism



[Fraunhofer Institute für Biomedizinische Technik]



[Dario, 2004]

[DeLuca, 1978]